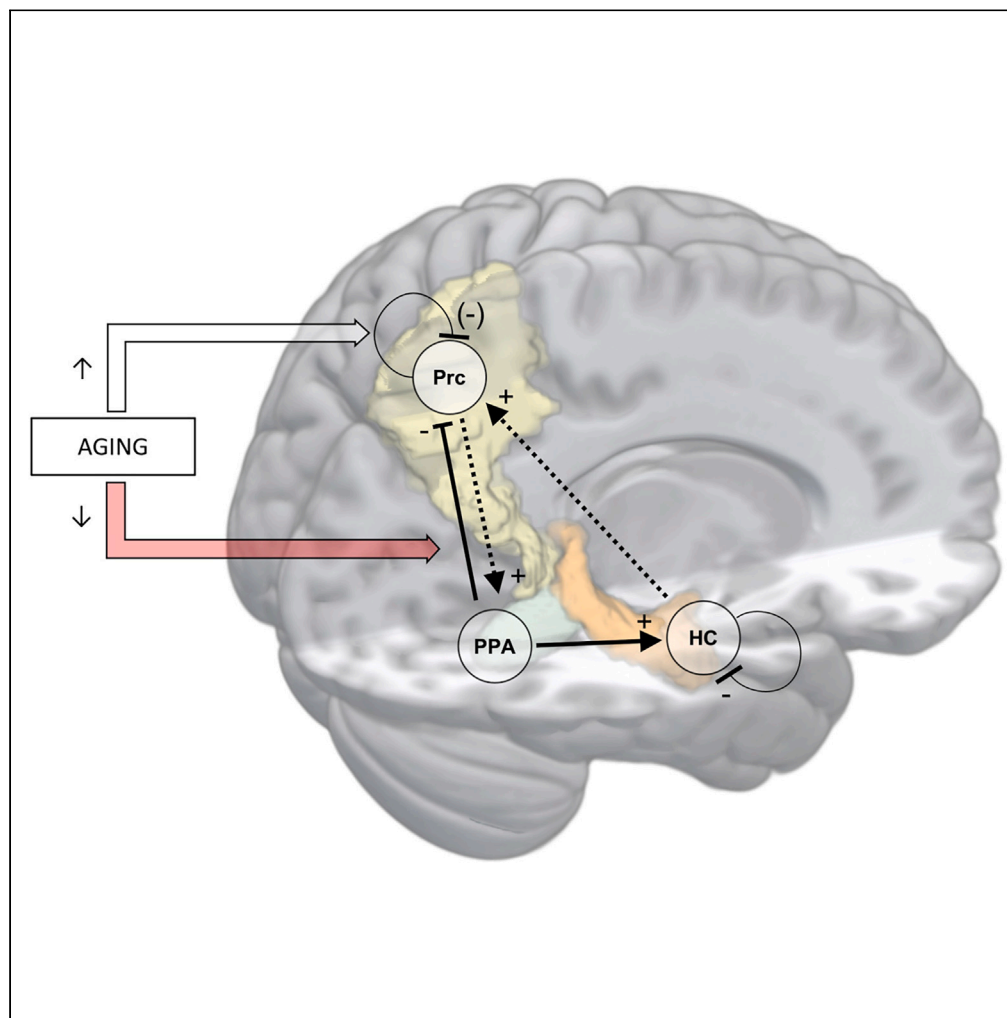


Article

Inhibitory temporo-parietal effective connectivity is associated with explicit memory performance in older adults



Björn H. Schott,
Joram Soch,
Jasmin M.
Kizilirmak, ...,
Gabriel Ziegler,
Magdalena
Sauvage, Anni
Richter

bjoern-hendrik.schott@dzne.de

Highlights

Older adults show reduced deactivations of the precuneus during memory encoding

Encoding-related temporo-parietal effective connectivity was modeled with DCM

Older adults exhibit reduced inhibitory connectivity from the PPA to the precuneus

Preserved inhibitory connectivity is associated with memory performance

Schott et al., iScience 26,
107765
October 20, 2023 © 2023 The
Author(s).
[https://doi.org/10.1016/
j.isci.2023.107765](https://doi.org/10.1016/j.isci.2023.107765)

Article

Inhibitory temporo-parietal effective connectivity is associated with explicit memory performance in older adults

Björn H. Schott,^{1,3,6,7,11,*} Joram Soch,^{1,2} Jasmin M. Kizilirmak,^{1,10} Hartmut Schütze,^{4,5} Anne Assmann,^{4,5} Anne Maass,⁴ Gabriel Ziegler,^{4,5} Magdalena Sauvage,³ and Anni Richter^{3,8,9}

SUMMARY

Successful explicit memory encoding is associated with inferior temporal activations and medial parietal deactivations, which are attenuated in aging. Here we used dynamic causal modeling (DCM) of functional magnetic resonance imaging data to elucidate effective connectivity patterns between hippocampus, parahippocampal place area (PPA), and precuneus during encoding of novel visual scenes. In 117 young adults, DCM revealed pronounced activating input from the PPA to the hippocampus and inhibitory connectivity from the PPA to the precuneus during novelty processing, with both being enhanced during successful encoding. This pattern could be replicated in two cohorts (N = 141 and 148) of young and older adults. In both cohorts, older adults selectively exhibited attenuated inhibitory PPA-precuneus connectivity, which correlated negatively with memory performance. Our results provide insight into the network dynamics underlying explicit memory encoding and suggest that age-related differences in memory-related network activity are, at least partly, attributable to altered temporo-parietal neocortical connectivity.

INTRODUCTION

One of the core questions in the cognitive neuroscience of episodic memory is why some experiences are encoded into stable memory traces that can subsequently be retrieved while other experiences are forgotten. In functional magnetic resonance imaging (fMRI) studies of episodic memory, this question is commonly investigated using the so-called subsequent memory approach.¹ Since its first application to fMRI,^{2,3} numerous studies have convergently shown that successful encoding robustly engages the medial temporal lobe (MTL) and particularly the hippocampus (HC), as well as inferior temporo-occipital regions like the parahippocampal place area (PPA), prefrontal, and lateral parietal cortices (for a meta-analysis, see⁴). On the other hand, structures of the cortical midline like the precuneus (Prc) and the medial prefrontal cortex (mPFC), which form part of the default mode network (DMN), are associated with relative deactivations during successful versus unsuccessful encoding.^{4,5}

Memory performance almost invariably declines with increasing age,⁶ and this decline is accompanied by characteristic alterations in memory-related network activations, including a reduced activation in inferior temporal cortices like the PPA and a reduced deactivation or even atypical activation of the DMN, and particularly cortical midline structures such as the Prc.^{5,7,8} Despite the robustness of these findings, the neural mechanisms underlying the relatively higher DMN activity during encoding still remain unclear. They may reflect increased reliance on DMN-dependent cognitive processes like self-referential or prior knowledge-dependent information during encoding⁵ or a reduced ability to suppress unwanted DMN activity, reflecting lower processing efficiency or specificity.^{9–11}

One potential mechanism mediating encoding-related hyperactivation of DMN structures in older adults could be increased excitatory or decreased inhibitory connectivity within the temporo-parietal memory network. The HC is highly interconnected with distributed neocortical regions,¹² and previous studies have highlighted both the importance of hippocampal-neocortical connectivity for successful memory formation^{13–18} and the susceptibility of memory-related network connectivity to age-related alterations.^{13,19}

¹German Center for Neurodegenerative Diseases (DZNE), Göttingen, Germany

²Bernstein Center for Computational Neuroscience (BCCN), Berlin, Germany

³Leibniz Institute for Neurobiology (LIN), Magdeburg, Germany

⁴German Center for Neurodegenerative Diseases (DZNE), Magdeburg, Germany

⁵Otto von Guericke University, Medical Faculty, Magdeburg, Germany

⁶Center for Behavioral Brain Sciences (CBBS), Magdeburg, Germany

⁷Department of Psychiatry and Psychotherapy, University Medical Center Göttingen, Göttingen, Germany

⁸German Center for Mental Health (DZPG), Magdeburg, Germany

⁹Center for Intervention and Research on adaptive and Maladaptive Brain Circuits Underlying Mental Health (C-I-R-C) Jena-Magdeburg-Halle, Magdeburg, Germany

¹⁰Neurodidactics and NeuroLab, Institute for Psychology, University of Hildesheim, Hildesheim, Germany

¹¹Lead contact

*Correspondence: bjoern-hendrik.schott@dzne.de

<https://doi.org/10.1016/j.isci.2023.107765>



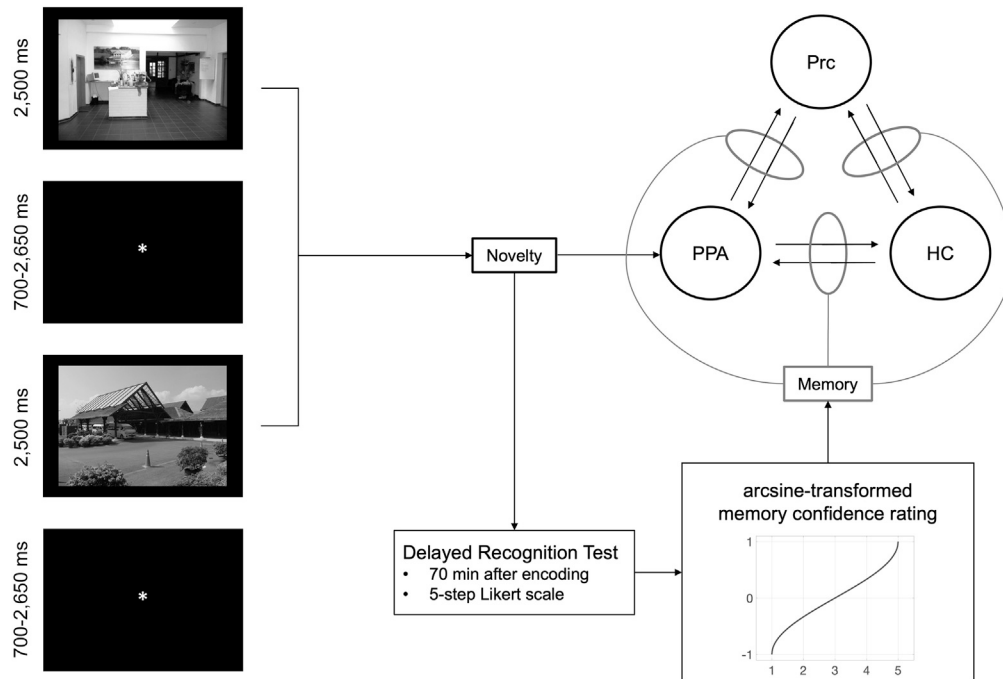


Figure 1. Experimental paradigm and design of the DCM study

During fMRI scanning, participants underwent an incidental visual memory paradigm. We used the novelty response to all novel pictures as driving input to the PPA and generated a parametric memory regressor by parametrically modulating the novelty response with the arcsine-transformed response in the delayed recognition task. The thus obtained memory regressor served as potential contextual modulator of the connections between the PPA, the hippocampus (HC), and the precuneus (Prc).

Most functional connectivity measures, however, do not normally allow inferences about the directionality of information flow or about its excitatory versus inhibitory nature. Such information can be deduced from analyses of *effective connectivity*, such as Granger causality analysis or dynamic causal modeling (DCM),²⁰ but these approaches have thus far rarely been used in the context of memory encoding in older adults. Results from previous studies suggest that prefrontal-hippocampal effective connectivity becomes less task-specific in older adults with memory impairment²¹ and that age-related deficits in HC-dependent navigation learning may be explained by higher HC excitability in older adults.²² However, no studies have thus far characterized the encoding-related information flow between the HC and the brain structures that show the most prominent age-related under-recruitment (i.e., inferior temporal structures involved in stimulus processing, and particularly the PPA) and over-recruitment (i.e., DMN structures, and particularly the Prc), respectively.

In the present study, we used DCM on fMRI data acquired during a visual memory encoding paradigm, in which novel photographs of scenes were presented intermixed with familiar scenes and encoded incidentally via an indoor/outdoor decision task. Memory was tested 70 min later via an old or new recognition memory task with a five-step confidence rating^{8,23,24} (Figure 1). Successful memory formation was associated with activation of the HC and the PPA as well as deactivation of the Prc in three independent cohorts (cohort 1: 117 young; cohort 2: 58 young, 83 older; cohort 3: 64 young, 84 older; see Table 1). In two cohorts that included both young and older adults, we could further replicate the previously reported age differences in memory encoding, with older adults showing reduced activation of the PPA but relatively increased activity in the Prc (Figure 2), while young and older adults showed comparable involvement of the anterior HC in successful encoding.⁵

Based on these findings, we analyzed patterns of effective connectivity between the HC and temporo-parietal memory network nodes using the parametric empirical Bayes framework.^{25,26} We constructed a DCM model that included the HC, the PPA, and the Prc as regions of interest (ROIs), exposure to novel stimuli as driving input to the PPA, and successful memory formation as a potential parametric modulator at each connection between the three ROIs (Figure 1). The PPA is thought to process and analyze the novel scene, binding its elements and incorporating the current context, which is then bound and encoded together by the HC.²⁷ Therefore, we first hypothesized that successful encoding would be associated with an up-regulation of information flow from the PPA to the HC. The Prc constitutes the core structure of a parietal memory network (PMN) proposed by Gilmore, Nelson, and McDermott.²⁸ The PMN has been associated with more pronounced responses to familiar compared to novel stimuli and with negative subsequent memory effects (or “subsequent forgetting effects”) in young adults,²⁹ which are attenuated or even inverted in older adults.⁵ Based on those observations, we further hypothesized that successful memory formation would be associated with a down-regulation of information flow (i.e., more pronounced inhibitory effective connectivity) to the Prc from either the PPA or the HC. With respect to age effects, we further hypothesized that at least one of the aforementioned mechanisms—i.e.,

Table 1. Demographic and behavioral data, MRI acquisition parameters

	Cohort 1	Cohort 2	Cohort 3
Demographics			
Young			
N	117	58	64
Age	24.37 (± 2.60)	23.62 (± 3.45)	24.45 (± 4.46)
Gender (f/m)	57/60	28/30	37/27
Older			
N	–	83	84
Age	–	65.20 (± 6.71)	62.96 (± 6.06)
Gender (f/m)	–	48/35	52/32
MRI parameters			
MRI scanner	Siemens Verio	Siemens Verio	Siemens Skyra
Number of slices	40	47	47
TR/TE/flip- α	2.40 s/30 ms/80°	2.58 s/30 ms/80°	2.58 s/30 ms/80°
Voxel size	2 × 2 × 3 mm	3.5 × 3.5 × 3.5 mm	3.5 × 3.5 × 3.5 mm
Scanning time	494.4 s	531.5 s	531.5 s
Unwarping	No	yes	yes
Memory performance			
Young A'	0.81 \pm 0.075	0.83 \pm 0.073	0.82 \pm 0.068
Older A'	N/A	0.78 \pm 0.072	0.77 \pm 0.077
Young versus older	N/A	t _{121.8} = 4.45; BF ₁₀ = 1417.21	t _{142.5} = 3.99; BF ₁₀ = 203.62

Data are shown separately for each cohort.

Abbreviations: N, sample size; f, female; m, male; TR, repetition time; TE, echo time; flip- α , flip angle; A', area under the curve in a ROC analysis of the recognition memory test, reflecting behavioral accuracy (hits versus false alarms).

enhanced information flow to the HC and inhibitory effective connectivity to the Prc—would be attenuated in older adults, which in turn would be associated with poorer memory performance within the group of older adults. To this end, we performed correlational analyses between connection strength and memory performance in the fMRI experiment (area under the curve, A')³⁰ and in additional, independent tests of explicit memory.

RESULTS

In the three independent cohorts, a characteristic pattern of novelty-related effective connectivity and encoding-related modulation could be identified. In cohorts 2 and 3, we could further observe age-related reductions in PPA-Prc effective connectivity that correlated with memory performance in the older participants.

Age differences in memory performance

Memory performance was defined as A', that is, the area under the curve plotting hits (i.e., correctly recognized previously seen images) against false alarms (i.e., new images incorrectly classified as previously seen), taking into account recognition confidence (see STAR Methods section for details). Table 1 (bottom) displays A' separated by cohorts and age groups. In cohorts 2 and 3, we found strong evidence for lower memory performance in older compared to young adults (cohort 2: t_{121.8} = 4.45; BF₁₀ = 1417.21; cohort 3: t_{142.5} = 3.99; BF₁₀ = 203.62). Gender did not have a robust effect on memory performance in any cohort or age group (all BF₁₀ < 0.91), with nominally opposing effects among the older adults of cohorts 2 and 3 (Table S1).

Activations and deactivations during novelty processing and memory encoding in young and older adults

Figure 2 displays representative activations and deactivations during novelty processing (novel versus familiar “master” images) and successful memory encoding (parametric memory regressor). An overview of novelty-related and memory-related fMRI activation maxima, separated by cohorts and age groups, is provided in Tables S2–S7.

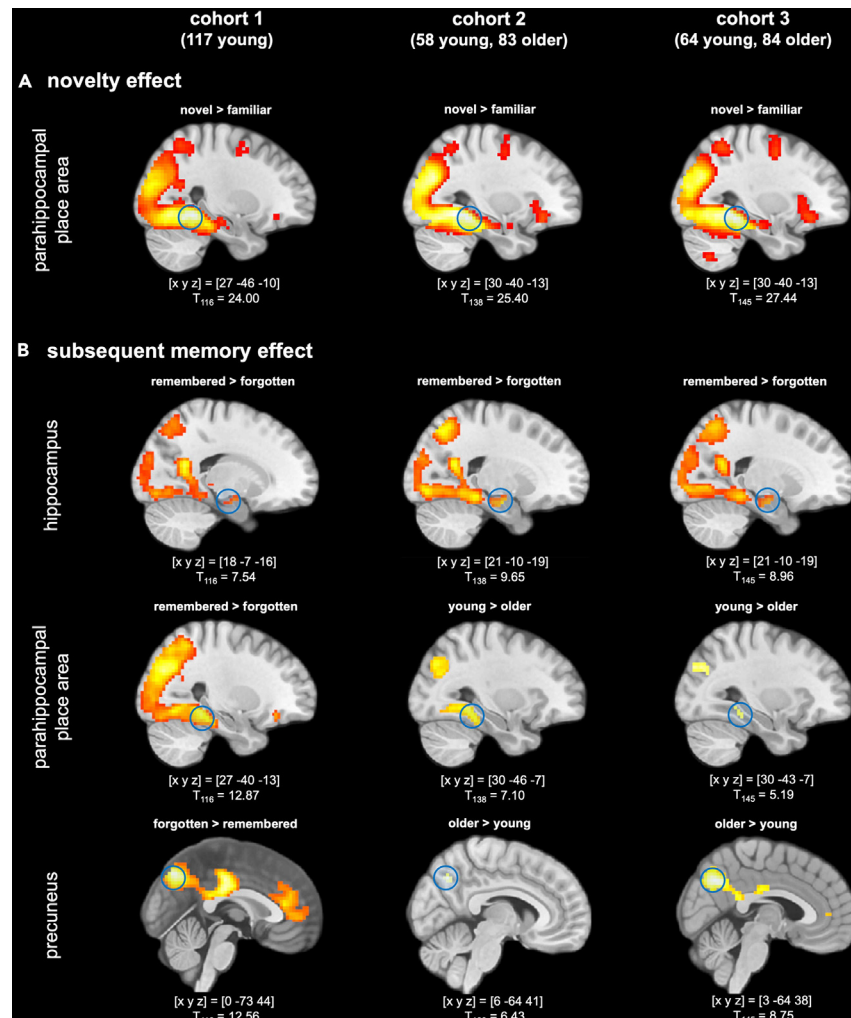


Figure 2. Neural correlates of novelty processing and successful encoding and their age-related differences

(A) Novelty effect. Across all cohorts and age groups, novelty processing (i.e., novel > familiar master images) was associated with increased activation of inferior temporo-parietal cortices, particularly the PPA, extending into the hippocampus.

(B) Subsequent memory effect. Top row: In all three cohorts, successful episodic memory formation elicited activation of the bilateral hippocampus (right hippocampus shown here). Middle row: Encoding-related activation of the PPA (left column) was reduced in older relative to young adults (middle and right columns). Bottom row: Encoding-related deactivations in the precuneus (left column) were reduced in older adults (middle and right columns). All contrasts are displayed at $p < 0.05$, FWE-corrected at voxel-level, minimum cluster size $k = 10$ adjacent voxels. Coordinates denote local maxima in the respective contrasts.

Novel compared to scene stimuli were associated with a robust fMRI response in the PPA (Figure 2, top row), replicating earlier findings with the same stimulus material.³¹ While PPA novelty responses were stronger in young compared to older adults in cohort 2, this finding could not be replicated at $p < 0.05$, FWE-corrected in cohort 3 (Tables S3 and S4).

Regarding the subsequent memory effect, we could replicate previously reported encoding-related activations and deactivations⁴ in all the cohorts (Tables S5–S7). In cohort 1, successful episodic memory encoding was associated with increased activation of the HC and an extensive temporal and inferior parietal network, including a pronounced local maximum in the PPA (Figure 2, left column). In cohorts 2 and 3, we additionally tested the age-related activation differences during successful encoding (Figure 2, middle and right columns; Tables S6 and S7). Replicating previous studies,⁵ we found older participants to exhibit lower activations in inferior and medial temporal structures, including the PPA, but relatively preserved encoding-related activation of the HC. Furthermore, in line with earlier studies, older adults exhibited reduced deactivations in midline structures of the DMN during successful encoding, with the maximum between-group difference in the right Prc in both cohorts 2 and 3 (Tables S6 and S7).

When explicitly testing for effects of gender, no activation differences survived our statistical threshold of $p < 0.05$, FWE-corrected with an extent threshold of 10 voxels in any of the three cohorts. In cohort 2, a single voxel in the rostral anterior cingulate showed a gender difference in the subsequent memory contrast, with women showing lower encoding-related deactivations compared to men.

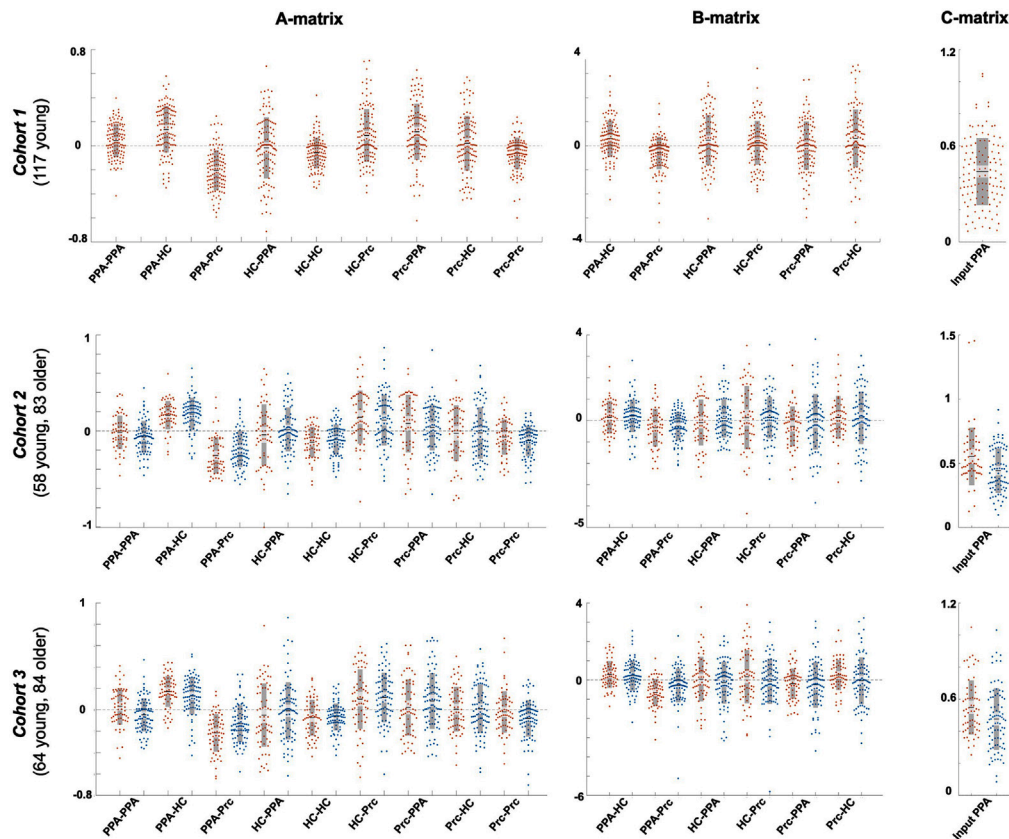


Figure 3. Distribution of DCM parameters across cohorts and single participants

A-matrix: intrinsic connections; B-matrix: contextual modulation by encoding success; C-matrix: driving input by novelty. Plots display means (solid black lines) \pm standard errors (light gray) and standard deviations (dark gray), along with all single data points (red: young adults, blue: older adults).

Locations of ROIs

ROIs of the PPA, the HC, and the Prc were selected based on both structural and functional anatomical constraints (for similar approaches, see ^{32,33}). The mean coordinate of the PPA ROI was located near [26 -47.5 -11], the HC ROI was centered approximately at [26 -13.5 -17.5], and the mean of the PPA ROI was around [7.3 -62.8 38.6] (for an illustration, see Figure S1). There was little variability within each cohort (all SD < 3 mm) and high agreement across all cohorts and age groups (Table S8).

Temporo-parietal effective connectivity and its modulation during memory encoding

The DCM parameters from the participants of each cohort are displayed in Figure 3, separated by age group for cohorts 2 and 3. Mean DCM parameters are shown in Table 2, separately for each cohort and age group. In every single participant, the driving input (i.e., the PPA response to novel stimuli) was positive (Figure 3, right panel), confirming the plausibility of choosing the PPA as input region.

Figure 4A displays the patterns of intrinsic connectivity of the temporo-parietal network (A-matrix) during novelty processing investigated in our DCM analyses, separated by main effects (top row) and age differences (bottom row). Connectivity changes related to successful memory formation (B-matrix) are displayed in Figure 4B, following the same layout as Figure 4A. Posterior connection strengths are displayed in Figure S2, highlighting connections that could be replicated across all three cohorts (or across cohorts 2 and 3 in case of age group effects).

Intrinsic connectivity between regions

Across all cohorts, there were pronounced excitatory connections from the PPA to the HC and from the HC to the Prc (Figure 3, left panel; Figure 4A, top row). A pronounced inhibitory connection was observed from the PPA to the Prc. All of these connections reached a posterior probability (PP) of 1.00 in all three cohorts (see also Figure S2, left panels) and exceeded a PP > 0.95 also when applying a free energy-based threshold. In cohorts 1 and 2, a positive connection was evident from the Prc to the PPA. In cohort 3, this connection reached a PP of >0.95 in older adults only.

Table 2. DCM parameters

	Cohort 1		Cohort 2		Cohort 3	
	Young		Young	Older	Young	Older
A-matrix						
PPA-PPA	0.043 ± 0.136		−0.014 ± 0.174	−0.063 ± 0.165	0.033 ± 0.171	−0.047 ± 0.154
PPA-HC	0.135 ± 0.193		0.165 ± 0.147	0.176 ± 0.168	0.172 ± 0.144	0.130 ± 0.174
PPA-Prc	−0.205 ± 0.167		−0.255 ± 0.189	−0.188 ± 0.189	−0.216 ± 0.174	−0.129 ± 0.174
HC-PPA	−0.019 ± 0.254		−0.041 ± 0.319	0.015 ± 0.229	−0.050 ± 0.296	−0.009 ± 0.268
HC-HC	−0.060 ± 0.128		−0.116 ± 0.158	−0.091 ± 0.158	−0.074 ± 0.168	−0.066 ± 0.125
HC-Prc	0.085 ± 0.219		0.144 ± 0.278	0.114 ± 0.266	0.100 ± 0.278	0.116 ± 0.232
Prc-PPA	0.115 ± 0.233		0.077 ± 0.300	0.036 ± 0.238	0.022 ± 0.263	0.084 ± 0.261
Prc-HC	0.020 ± 0.227		−0.025 ± 0.291	−0.022 ± 0.266	0.006 ± 0.209	0.011 ± 0.228
Prc-Prc	−0.064 ± 0.132		−0.063 ± 0.183	−0.102 ± 0.157	−0.020 ± 0.193	−0.079 ± 0.170
B-matrix						
MEM_PPA-HC	0.293 ± 0.762		0.154 ± 0.759	0.211 ± 0.758	0.284 ± 0.694	0.224 ± 0.777
MEM_PPA-Prc	−0.306 ± 0.669		−0.334 ± 0.878	−0.262 ± 0.671	−0.656 ± 0.704	−0.283 ± 0.880
MEM_HC-PPA	0.232 ± 1.050		−0.100 ± 1.071	0.102 ± 0.893	0.041 ± 1.154	−0.140 ± 1.089
MEM_HC-Prc	0.121 ± 0.908		0.131 ± 1.476	0.135 ± 0.974	0.166 ± 1.378	−0.072 ± 1.173
MEM_Prc-PPA	−0.003 ± 1.004		−0.274 ± 0.932	−0.062 ± 1.298	−0.195 ± 0.786	−0.257 ± 1.187
MEM_Prc-HC	0.306 ± 1.195		0.144 ± 0.995	0.122 ± 1.226	0.261 ± 0.785	−0.040 ± 1.219
C-matrix						
Input_PPA	0.439 ± 0.209		0.553 ± 0.224	0.443 ± 0.173	0.549 ± 0.169	0.476 ± 0.192

Mean DCM parameters ± standard deviations are shown separately for each cohort and age group. A-matrix: intrinsic connections. B-matrix: contextual modulations by successful encoding. C-matrix: driving input (novelty-related activation of the PPA).

Intrinsic inhibitory self-connectivity

In the DCM framework, self-connectivity is *a priori* expected to be inhibitory, with higher negative values reflecting stronger (self-)inhibition.³⁴ Self-connectivity is reflected in the diagonals of the matrices in Figure 4A (top row). Across all three cohorts, we observed robust negative self-connectivity of the HC (Figure 4A, top row; Figure S2, left panels), most likely reflecting reduced auto-inhibition (relative to the implicit baseline) during processing of the novel stimuli, which served as driving input. No replicable pattern emerged with respect to the self-connectivity of the PPA or the Prc.

Memory-related connectivity changes (contextual modulations)

Successful encoding, as captured by the parametrically modulated memory regressor, was associated with increased effective connectivity from the PPA to the HC and more pronounced negative effective connectivity from the PPA to the Prc (Figure 3, middle column; Figure 4B, top row). These connectivity changes could be replicated in all three cohorts at a marginal PP > 0.95, and the negative PPA-Prc connection also reached a PP > 0.95 in all three cohorts when applying a free energy-based threshold (Figure S2, left panels, red bars). Additionally, in cohort 1, we observed increased bidirectional encoding-related effective connectivity between the HC and the Prc, but in cohorts 2 and 3, these parameters did not exceed the *a priori* defined threshold of PP > 0.95.

Age-related difference in memory network effective connectivity

As there were no older adults in cohort 1, all age differences reported here are based on cohorts 2 and 3. In both cohorts, age group was associated with more positive (i.e., reduced inhibitory) effective connectivity from the PPA to the Prc (Figures 4A and 4B, bottom rows; Figure S2, right). This reduced inhibitory temporo-parietal effective connectivity was found in the A-matrix (intrinsic connection) in both cohorts, and, additionally, in cohort 3, it was also found in the B-matrix (memory-related contextual modulations). Furthermore, even though there was no clear age-independent pattern (see section “reduced memory-related deactivations of the Prc in older adults”) of Prc self-connectivity across the three cohorts, inhibitory Prc self-connectivity was nevertheless reduced in older adults compared to young adults in both cohorts 2 and 3.

Association of effective connectivity with memory performance in older adults

As described earlier, the inhibitory connection from the PPA to the Prc was attenuated in older compared to young adults (Figure 4A, bottom row; Figure S2, right panels). We therefore focused on this connection when testing for a relationship between DCM parameters and memory

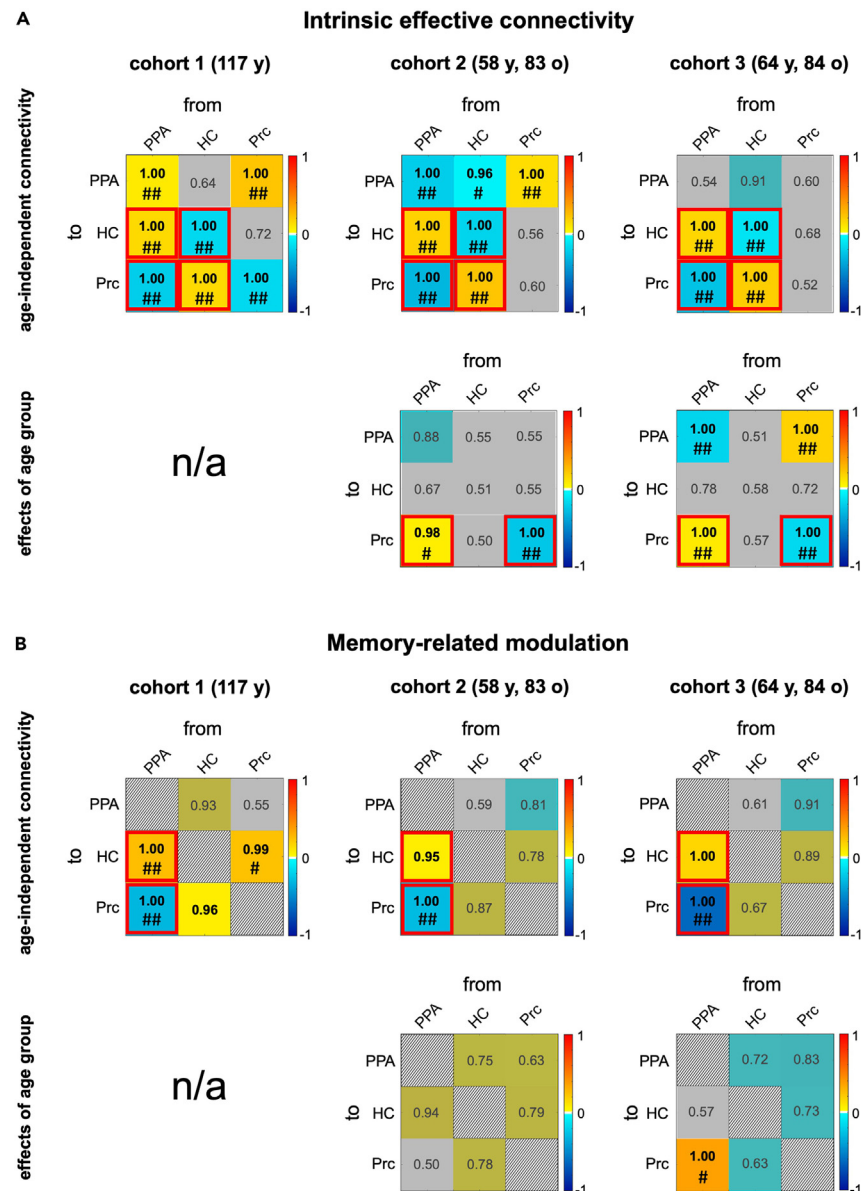


Figure 4. Connectivity matrices of effective connectivity strengths and their modulation by age group

(A and B) Intrinsic connections and (B) contextual modulations. Color denotes the connection strength, reflecting positive (“excitatory”; warm colors) versus negative (“inhibitory”; cool colors) connectivity for main effects and higher versus lower values in older adults for age effects (scaled from -1 to 1 at all instances to improve comparability across cohorts). The posterior probability (PP) of a parameter being >0 in absolute value is shown for each connection; connections with PP < 0.95 are gray-shaded. Hashtags denote free energy-based evidence; # free energy-based PP > 0.75 (“positive evidence”); ## free energy-based PP > 0.95 (“strong evidence”).

performance in older adults. Outlier-robust Shepherd’s *Pi* correlations,³⁵ adapted for Bayesian statistics,³⁶ were computed between the PPA-Prc connection strength and *A'* as a measure of memory performance (see [STAR Methods](#) section for details). In both cohorts (2 and 3), the parameter representing PPA-Prc connectivity was negatively correlated with *A'* (cohort 2: $\Pi = -0.368$, $BF_{10} = 18.21$; cohort 3: $\Pi = -0.297$, $BF_{10} = 2.63$; [Figure 5A](#)), such that stronger PPA-Prc inhibitory connectivity was related to better memory performance.

We then computed exploratory Bayesian Shepherd’s *Pi* correlations for *A'* and all DCM parameters in young and older adults ([Figure 5B](#)). In older adults of both cohorts, we found replicable evidence only for the correlation with the PPA-Prc connection. In young adults, evidence in favor of a correlation between the PPA-Prc connection and *A'* was found in cohort 3 ($\Pi = -0.317$, $BF_{10} = 2.01$), but not in cohorts 1 and 2 (all $BF_{10} < 0.23$). On the other hand, the driving input (C-matrix, i.e., the PPA novelty response) was correlated positively with *A'* in young adults in cohorts 1 and 3, but not in older adults. Calculating cumulative Bayes factors as the Bayes factors for the averaged correlation coefficients

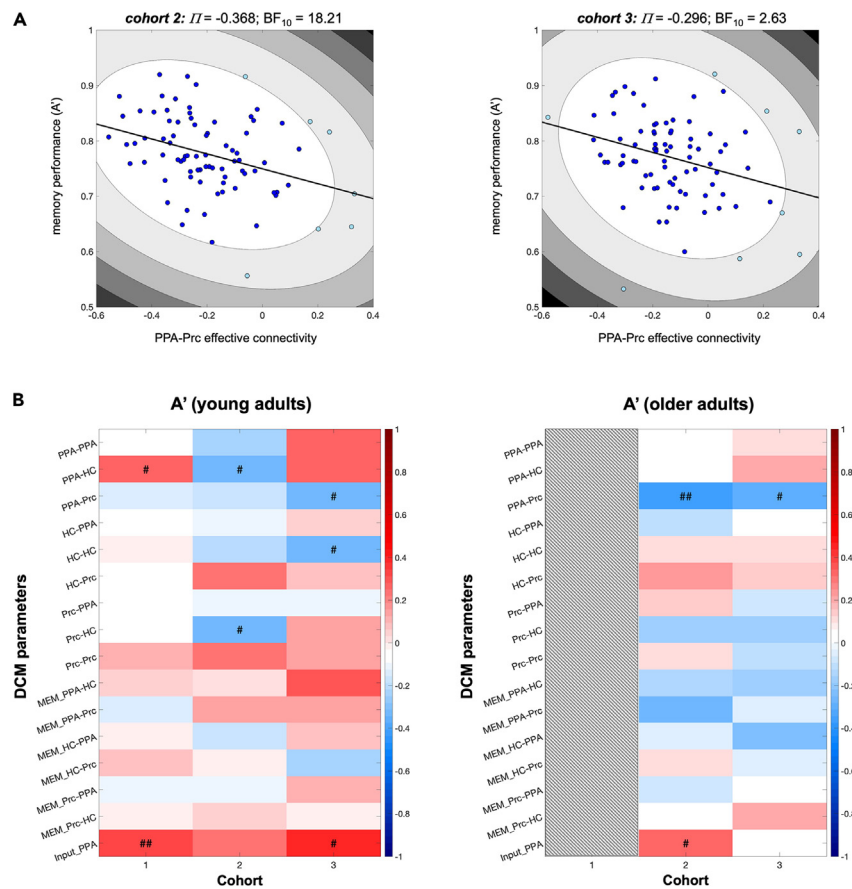


Figure 5. Correlations between DCM parameters and memory performance

(A) Plots depict outlier-robust Bayesian Shepherd's P_i correlations between the inhibitory PPA-Prc connection in older adults in cohorts 2 and 3. (B) Results from pairwise Bayesian Shepherd's P_i correlations of the individual participants' DCM parameters with memory performance (A') in young (left) and older (right) participants, separated by cohort. Positive and negative correlations are shown in red and blue, respectively. # $BF_{10} > 2.00$; ## $BF_{10} > 10.00$.

(weighted for effective sample sizes; the effective sample size was defined as the sample size remaining after exclusion of (1) missing data points from individual participants [e.g., due to skipping of the 24 h delayed recall] and (2) the Bootstrap-based outlier exclusion implemented in the Shepherd's P_i correlation) confirmed the observation of correlations between the driving input and A' in young adults and between the PPA-Prc connection and A' in older adults (all cumulative $BF_{10} > 400.0$). The cumulative evidence for a relationship between the PPA-Prc connection and A' in young adults, on the other hand, was limited ($BF_{10} = 3.96$; Tables S9 and S10).

Finally, we tested for a potential relationship between DCM parameters and measures of memory in independent—verbal—memory tests, the verbal learning and memory test (VLMT)³⁷ and the Logical Memory subscale of the Wechsler Memory Scale (WMS).³⁸ No correlations of DCM parameters with those measures of memory performance were directly replicable across cohorts for either age group. In the cumulative statistics, there was evidence for a relationship between VLMT and WMS performance (learning and delayed recall) and the driving input in older, but not in young adults, but the evidence was substantially lower ($15.0 < BF_{10} < 19.8$; Figure S3; Tables S9 and S10).

DISCUSSION

In the present study, we have used DCM to elucidate the putative temporo-parietal information flow underlying fMRI activations and deactivations during successful memory formation and their characteristic age-related differences. We found that successful memory encoding was associated with increased PPA-hippocampal effective connectivity and increased inhibitory effective connectivity from the PPA to the Prc in both young and older adults. In older adults, the inhibitory connection from PPA to Prc was, however, reduced, and less negative inhibitory—or even positive—PPA-Prc connectivity was associated with poorer memory performance.

Cortical-hippocampal interactions during novelty processing and memory encoding

In three independent cohorts, a characteristic pattern of intrinsic effective connections emerged, which were in part further modulated as a function of encoding success (for an overview, see Figure 6). Most prominently, the following connections were observed:

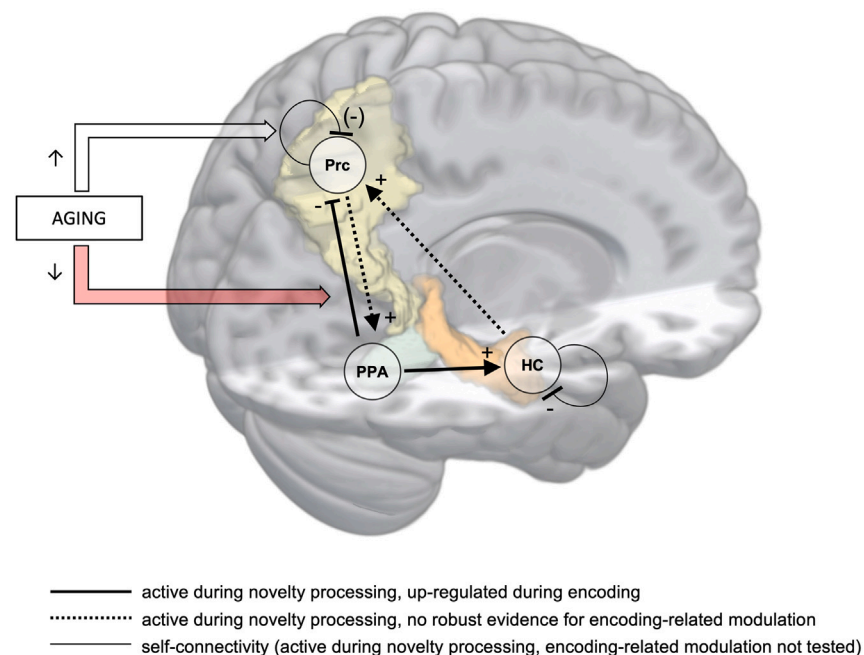


Figure 6. Temporo-parietal effective connectivity during novelty processing and successful memory encoding

Successful encoding was associated with increased activation of the hippocampus by the PPA and stronger suppression of the precuneus by the PPA. In older adults, the inhibitory connection from PPA to precuneus was attenuated and related to worse memory performance.

The PPA exerts novelty-related excitatory input on the HC, which is up-regulated during successful encoding

Previous studies have demonstrated that both the HC and the PPA exhibit robust responses to novel scenes^{39,40} as well as subsequent memory effects.^{30,41} The direction of information flow from the PPA to the HC observed in the present study suggests that HC-dependent encoding of the stimuli occurs *after* higher-level perceptual analysis of the scene stimuli in the PPA. This interpretation is supported by previous neuroimaging studies^{27,42} as well as by electrophysiological investigations and immediate-early gene imaging studies in rodents, which, despite the lack of a clearly defined homologue of the PPA in rodents, support the notion that scene processing is mediated by the parahippocampal cortex⁴³ and that hippocampal encoding of episodes is preceded by stimulus processing in inferior-medial temporal cortices.^{44,45}

The HC shows negative self-connectivity during novelty processing

Self-connectivity is *a priori* defined as negative within the DCM framework,³⁴ with negative self-connectivity reflecting the release of auto-inhibition. Negative self-connectivity of the HC upon driving input (here: activation of the PPA to novel scene stimuli),⁴⁶ in our view, thus most likely reflects hippocampal novelty responses to the scene stimuli. The HC exhibits strong responses to novel stimuli,^{47,48} a finding also replicated in another cohort of older adults using the same paradigm as in the present study.^{49,50} Hippocampal self-connectivity was not influenced by age group in our study. Age-related changes in intra-hippocampal connectivity have been reported using different methodologies, although results are not entirely conclusive. While a DCM study on navigational learning found reduced hippocampal auto-inhibition in older adults,²² results from longitudinal resting-state fMRI investigations suggest an age-dependent decrease of voxel-wise functional connectivity in the anterior HC but a connectivity increase in the posterior HC.⁵¹ A limitation of our present study is that we did not allow for a modulation of self-connections by successful encoding in our model, as the self-connections of the PPA and Prc did not replicate consistently across cohorts (Figure 4). We can therefore not exclude a potential age-dependent modulation of hippocampal self-connectivity during successful encoding.

The PPA exerts inhibitory input to the Prc during novelty processing and successful encoding

Deactivations of the Prc are a common finding in studies using the subsequent memory effect,^{4,29} and a straightforward explanation for this is that the Prc as a DMN structure deactivates during most tasks that require externally directed attention,⁵² including novelty processing⁵⁰ and successful encoding.^{5,24} During encoding of novel stimuli, it may be of particular importance to suppress processing related to retrieval and familiarity, which engages the Prc.^{4,28,53} While the function of the Prc in explicit memory processes likely goes beyond supporting retrieval (see section “[further limitations and directions for future research](#)”), it is notable from the present results that suppression of Prc activity during novel stimulus processing and successful encoding was not found to be mediated by the HC, but rather directly by the PPA, bypassing the HC.

The HC exerts excitatory input to the Prc during novelty processing

Unlike the PPA, the HC exerted positive input to the Prc during processing of novel stimuli, although there was only very limited evidence for a further modulation by encoding success (Figures 3, 4, and S2). One explanation for this may be that the hippocampal novelty signal is relayed to the Prc, allowing for novelty-related deactivation²⁸ (section “further limitations and directions for future research”).

The Prc exhibits positive effective connectivity to the PPA during novelty processing

In cohorts 1 and 2 and in the older participants from cohort 3, we further found an excitatory connection from the Prc to the PPA. The Prc is strongly interconnected with the parahippocampal cortex,⁵⁴ of which the PPA is a subregion. Projections from the Prc to the parahippocampal cortex are thought to be of a feed-backward type. One possible function of this connection could be that the Prc provides information based on existing knowledge that can be used to integrate elements of a novel scene into existing memory representations (for a detailed discussion, see section “further limitations and directions for future research”).

Reduced memory-related deactivations of the Prc in older adults

The DMN, and particularly the Prc, typically shows activations during episodic retrieval, but deactivations during encoding of novel stimuli⁴ (for a potentially differential role of the Prc during encoding of repeatedly presented information, see below). It thus seems plausible to assume that, during processing of novel stimuli, suppressing Prc activity may help to reduce interference with familiar information.²⁸ The results of our DCM analysis point to the presence of a direct inhibition of the Prc by the PPA during processing of novel stimuli, which is further enhanced during successful encoding and attenuated in older compared to young adults (Figure 6). We therefore tentatively suggest that the commonly observed attenuated encoding-related DMN deactivation in older adults—and especially in those with poor memory performance—^{5,24} may result from a reduced ability to suppress ongoing DMN activity during novelty processing and successful encoding.

This interpretation may be somewhat at odds with the commonly proposed notion that increased activation of parietal—and also prefrontal—neocortical structures may reflect a compensatory mechanism for diminished MTL function in old age.^{5,55} One possible interpretation for this apparent discrepancy is that compensatory activity might be particularly relevant in older adults with pre-clinical or subclinical memory impairment. While preserved patterns of memory-related brain activity (i.e., patterns with high similarity to those of young adults) have been associated with better memory performance in older adults,^{8,30,56,57} those with poorer memory performance can show not only deactivations but even atypical activations of DMN structures during successful versus unsuccessful encoding,⁵ possibly reflecting an increased reliance on self-referential or prior knowledge-dependent information during encoding.^{58–60} In line with this interpretation, increased activity of midline brain structures during novelty processing and successful memory encoding has been reported in individuals at risk for Alzheimer’s disease (AD), that is, otherwise healthy older adults with subjective cognitive decline (SCD)⁵⁰ or cognitively unimpaired older individuals with increased beta-amyloid deposition as assessed with PET.⁶¹ Notably, this DMN hyperactivation is no longer observed in patients with early-stage AD,⁵⁰ suggesting that, whether compensatory or not, it is nevertheless vulnerable to more pronounced disruption of brain function. Whether DMN hyperactivation reflects compensatory mechanisms at a pre-clinical stage that break down during disease progression or rather a more general impairment of inhibitory processes that precedes a broader decline in neural function should be further elucidated in future studies.

The relationship between inhibitory connectivity and memory performance

In our present study, only the inhibitory connection from the PPA to the Prc was associated with memory performance in older adults, whereas evidence for an association of that connection with memory performance in young adults was limited (Figure 5; Tables S9 and S10). This suggests that neocortical inhibitory mechanisms, in addition to altered hippocampal connectivity,²¹ contribute to age-related reduced efficiency of memory networks. This does not rule out that connectivity of the HC with other (e.g., prefrontal) brain regions may also be associated with memory performance. Nyberg and colleagues, for example, showed that higher connectivity of the ventrolateral PFC and the HC during encoding was associated with higher dropout rate from a longitudinal study, as a proxy for worse cognitive and clinical outcomes.²¹ Furthermore, a study on hippocampal-posterior neocortical effective connectivity during spatial navigation suggested that reduced hippocampal auto-inhibition was associated with lower learning performance in older adults.²² Despite the heterogeneity of the models and ROIs across those studies and our present study, we suggest that our findings nevertheless converge with the aforementioned results in highlighting, more generally, the role of inhibitory connectivity within the extended memory networks in successful aging of human memory systems.

It should further be noted that age-related activation increases in brain structures not typically involved in the task at hand have also been observed in cognitive domains other than explicit memory,⁶² and even in the motor system.⁶³ As, in the latter study, ipsilateral motor system activity did not predict better performance (e.g., reaction times), the authors suggested that their results speak against a compensatory role of age-related task-related hyperactivations. Together with our present results, we suggest that loss of inhibitory activity might constitute a cross-domain mechanism of brain aging, and future research should further explore its possible relationship with subclinical pathology.

The multifaceted role of the Prc in human long-term memory

The engagement of DMN structures during memory retrieval processes is a well-replicated finding,^{52,53} and the Prc, in particular, is well-known for its role in episodic retrieval,⁴ despite an ongoing debate with respect to a preferential role in recollection versus familiarity.^{28,64} Irrespective of the type of retrieval process involved, it seems plausible to assume that, during processing of novel stimuli, suppressing

Prc activity may help to reduce interference with familiar information. In line with this interpretation, Gilmore and colleagues proposed a PMN that includes the Prc, which deactivates in response to novel information and shows increased responses as a function of stimulus familiarity.²⁸ During successful encoding, higher activity in ventral parietal structures has been associated with subsequent forgetting rather than remembering.^{4,28,29} On the other hand, there has also been evidence for higher activity in dorsal parietal structures associated with positive subsequent memory effects.²⁹ While the meta-analysis by Uncapher and Wagner was focused on lateral parietal structures, a similar pattern of functional heterogeneity has also been proposed for midline parietal subregions of the DMN.⁶⁵ Particularly the dorsal Prc is involved in switching between DMN activity and activity of task-positive networks⁶⁶ and has been shown to be actively engaged in some attention-demanding tasks, possibly mediating the integration of inwardly directed and externally directed cognitive processes.⁶⁷ More recently, the Prc has also been proposed as a key region involved in memory acquisition, particularly for visuo-spatial material.^{68–70} However, those studies all used repeated stimulus exposure and may therefore reflect a primarily neocortically mediated form of learning distinct from HC-dependent memory for unique episodes.^{71,72}

One possibility to reconcile those findings with the results of our present study is that the Prc may serve, to some extent, as a gatekeeper during long-term memory formation, enabling the parallel storage of unique episodes in their spatial and temporal context and of elaborate and multiply associated information (i.e., schemas).^{71,73} More broadly, future research should explore the possibility that PMN structures may contribute to the distinction of episodic and semantic memory.⁷⁴

Associations of the driving input with memory performance

While, in young adults, we found only limited evidence for association between PPA-Prc inhibitory connectivity and memory performance, the combined analyses across cohorts point to very strong evidence for a positive relationship between the driving input to the PPA and memory performance in young adults (A'; see Table S10). In older adults, such a relationship was not found for A', but there was moderate evidence for a positive association between learning and delayed recall performance in the WMS and, to some extent, also in the VLMT (Table S9).

With respect to our present results, we tentatively suggest that the most straightforward observation for the correlations observed here is that C-matrix in our DCM design essentially reflects the novelty response in the PPA. Previous analyses of our data set suggest that a higher similarity of the whole-brain novelty and memory responses with the prototypical responses in a reference sample of healthy young adults is associated with better memory performance in both the experimental task itself and also in the WMS and VLMT.^{30,57} There were a few differences in details between the correlations here and those reported in our previous works (e.g., overall stronger correlations of the memory-based scores with memory performance, particularly in younger adults), and we suggest that they most likely reflect the definition of the underlying fMRI measures (whole-brain single-value scores versus the peak novelty response in the PPA), which, despite likely showing high covariance, nevertheless constitute distinct measures of brain activity. According to this interpretation, the observed correlations between the driving input and the performance in independent memory tests in older adults may reflect the previously described associations between the overall integrity of fMRI response patterns and cognitive function, particularly memory performance.^{56,57}

Feasibility and limitations of replication in DCM studies

Beyond the specific implications for cognitive neuroscience of the aging memory system, our present study also concerns the critical issue of replication in human fMRI research.⁷⁵ While recent analyses suggest that the replicability of group-level fMRI results is overall encouraging when a study is adequately powered,^{76,77} few studies have so far addressed the issue of replication in DCM, and even less so, in the context of the parametric empirical Bayes (PEB) framework used here. Earlier DCM studies describing replications or addressing the issue of reproducibility have commonly reported results from Bayesian model selection in combination with classical statistical tests (e.g., t-tests) on the individual participants' DCM parameters^{78–80} or even fully relied on classical statistical testing at group level.⁸¹ In the present study, we observed highly reproducible patterns of intrinsic connectivity in four parameters of the A-matrix (intrinsic connectivity during novelty processing; see Figure 4A, top row), all of which remained in the model when applying the more stringent free energy-based threshold. On the other hand, self-connections, particularly those of the PPA, showed considerable inconsistencies, even with robust effects in opposite directions across cohorts (Figure 4A). This observation points to a potentially underappreciated difficulty in robustly modeling self-connections, which might also explain the rather low rate of reporting self-connectivity in neuropsychiatric DCM studies (approximately 25%).⁸² Thus, we did not include a modulation of self-connectivity in our model space, as we found it difficult to generate hypotheses on the modulation of self-connections that showed no robust intrinsic pattern.

In the B-matrix (contextual modulation by successful encoding), the enhanced negativity of the PPA-Prc connection could be replicated at free energy-based PP > 0.95 (Figure 4B, top row). The increased positivity of the PPA-HC connection was robust at PP > 0.95 (free energy-based) in cohort 1 (which consisted of young participants only), whereas this connection was reliable only at marginal PP in cohorts 2 and 3 (which included approximately 57% older adults). One reason for this may be that the free energy threshold is based on iterative pruning of parameters from the model based on the posterior covariance among parameters.²⁶ This procedure is highly effective for the selection of the most parsimonious models, but, in the context of replication, one should consider the possibility that subtle differences in the strengths of parameters with high covariance across cohorts may result in differential pruning, which might, in extreme cases, result in an apparent replication failure when considering free energy-based thresholds only. Between-group differences might also explain the inconclusive findings regarding the bidirectional positive modulation of HC-Prc connectivity observed in cohort 1. Despite showing nominally positive parameters in cohorts 2 and 3, these connections did not pass the *a priori* defined threshold of PP > 0.95 in these cohorts (Figure 4B). In addition to the

inclusion of older participants, the differences in trial timings and scanning parameters (Table 1) might constitute factors that could potentially impair robust replication.

In addition to the DCM parameters themselves, replicability is also important with respect to their correlation with behavioral measures. While we found negative correlations between PPA-Prc connectivity and memory performance in the older adults of both cohorts 2 and 3, the strength of evidence between the cohorts was different, despite similar magnitudes of the correlation coefficients (Figure 5A). Here we aimed to implement a meta-analytic approach to obtain cumulative Bayesian inference across cohorts (Nikolakopoulos and Ntzoufras, 2021; see Tables S9 and S10), but we acknowledge that there is an ongoing methodological debate on cumulative Bayesian inference^{83–85} and that further validation of the method used here is warranted. This is of particular importance with respect to the correlations with independent measures of memory, for which evidence was found only in the cumulative statistics (Table S9). Furthermore, additional replication approaches to assess the robustness of brain-behavior correlations in DCM, such as bootstrapping,⁸⁶ should be considered in future studies.

Interpretation of DCM results at the neuronal level

While the results of our DCM analyses could be robustly replicated in three independent cohorts, it must nevertheless be acknowledged that the DCM approach relies on multiple highly complex assumptions regarding functional neuroanatomy (see section “associations of the driving input with memory performance”), model space, and model selection,^{87,88} as well as the underlying biophysical mechanisms when inferring on a neuronal state from a hemodynamic signal.⁸⁸ In the present study, we interpreted our main finding, such that the PPA exerts inhibitory activity onto the Prc during novelty processing, which is further increased during successful episodic encoding and attenuated in aging. More generally, we have used DCM to infer on information flow between brain areas in relation to a driving input (novelty) and a behavioral outcome (remembered versus forgotten), contextually modulating connections between regions. Information flow in this context can be thought of as the first region passing on information to the second region (by causing it to receive different inputs as a function of the contextual modulator). Similarly, a region can be thought of as acting inhibitory or excitatory on a target area, if the strength of its connection to this area is negative or positive, respectively, in line with widely accepted interpretations of DCM.⁸⁸

Thus, it must be noted that, when referring to inhibitory activity in the interpretation of our present results, we refer to large-scale network dynamics, not small-scale regional perturbations. We acknowledge that great care must be taken when interpreting the results of DCM for fMRI data with respect to the underlying neuronal processes, particularly at the microcircuit level. One promising approach for future improvement is to use more elaborate models of the underlying neurovascular coupling and resulting BOLD signal,^{89–91} which can, in principle, be incorporated into DCM analysis.⁹²

Conclusions

Using DCM on fMRI data acquired during a visual memory encoding task, we could demonstrate that successful memory formation is associated with increased information flow from the PPA to the HC and suppression of information flow from the PPA to the Prc. A preserved inhibitory PPA-Prc connection was associated with better memory performance in two cohorts of healthy older adults, suggesting that, in addition to age-related changes in hippocampal connectivity, neocortical connectivity changes should also be considered. Our results highlight the importance of inhibitory mechanisms in successful aging of the human memory system. Future studies should investigate the longitudinal trajectories of inhibitory processes in human explicit memory, in order to explore the possibility that impaired inhibition might constitute an early pathophysiological mechanism in the development of age-related cognitive decline.

Limitations of the study

ROIs and the comparability of DCM studies

A limitation of the present study is inherent to the DCM approach, that is, the restriction to the *a priori* selected regions included in the model.⁸⁷ In the present study, we performed a rather rigid ROIs definition, based on anatomical constraints, literature-based assumptions, and fMRI activations, similar to a previously described approach³³ (see STAR Methods). While this approach yielded highly consistent ROI locations across cohorts and age groups (Table S8), the choice of ROIs nevertheless differed from those used in previous DCM studies.^{21,22,93} Most critically, our model did not include prefrontal cortex regions, which are typically involved in successful episodic encoding.⁴ One reason for this was that the focus of our study was on the Prc, which showed the most robust age-related activation difference (Figure 2; Tables S6 and S7). Furthermore, encoding-related prefrontal activation clusters were distributed across several frontal lobe structures and showed variability across cohorts, such that the selection of one given prefrontal ROI might have been to some extent arbitrary. We can therefore not exclude that prefrontal connectivity may additionally contribute to memory performance in older adults, as suggested in earlier studies.^{21,94}

Within the HC, we restricted our ROI to the anterior HC. This was motivated by previously reported associations between anterior hippocampal structure and function with age-related memory decline^{21,95} and on the aim to avoid an overlap with the PPA ROI, but we acknowledge that investigating differential connectivity patterns along the hippocampal axis will likely provide further important information on the aging HC-dependent memory system.⁹⁶

Another limitation related to our ROI selection concerns the choice of the PPA as input region. While it is plausible to use either early visual cortex regions^{21,22,93} or stimulus-responsive brain structures (e.g., the fusiform face area in a face-name encoding task^{21,22,93}), this may limit the generalizability of the resulting models to other cognitive tasks. In the present study, for example, the observed association between PPA-Prc connectivity and memory performance did not generalize to independent, verbal, memory tasks (Figure S3; Table S9), which suggests that the

specific association of PPA-Prc effective connectivity with memory performance may be limited to visual or spatial memory. In the combined analyses across cohorts, there was some evidence for an association between the driving input to the PPA during novelty processing and memory performance in the independent tests in older adults. Please see the [discussion](#) for a more detailed discussion of this observation.

Further limitations and directions for future research

Beyond ROI selection, it must be noted that the DCM approach relies on complex assumptions with respect to functional neuroanatomy (see above), model space, and model selection,^{87,88} but also the underlying biophysical mechanisms when inferring on a neuronal state from a hemodynamic signal.⁸⁸ It is thus likely overstated to assume direct causality from the effective connectivity patterns observed, and we are aware that our model, its reproducibility aside, is most likely incomplete (for a more detailed elaboration, see [discussion](#), section [interpretation of DCM results at the neuronal level](#)).

Another limitation of the present study may result from the sampling of the study cohort³⁰ and the lack of AD-related biomarkers. Despite the considerable interindividual variability in memory performance among the older adults in our cohort²⁴ ([Figure 2](#)), it must be acknowledged that older participants were most likely healthier than average. This was both due to our participant recruitment strategy, which led healthy and active older adults to more likely volunteer for participation (see [STAR Methods](#)), and due to the exclusion of participants with severe comorbidity.³⁰ In a large cohort that included older adults with SCD and mild cognitive impairment (MCI) as well as manifest AD, novelty-related Prc responses were found to exhibit an inverse U-shaped pattern from healthy older adults over SCD and MCI to manifest AD.⁵⁰ It remains thus to be determined whether the association between temporo-parietal inhibitory connectivity and memory performance also applies to individuals with memory impairment or dementia risk states. Furthermore, future studies should also follow-up older adults with memory impairment longitudinally to assess whether progressive memory decline might be associated with decreasing inhibitory connectivity over time.

STAR★METHODS

Detailed methods are provided in the online version of this paper and include the following:

- [KEY RESOURCES TABLE](#)
- [RESOURCE AVAILABILITY](#)
 - Lead contact
 - Materials availability
 - Data and code availability
- [EXPERIMENTAL MODEL AND STUDY PARTICIPANT DETAILS](#)
 - Participants
 - Informed consent and ethics approval
- [METHOD DETAILS](#)
 - Experimental paradigm
 - MRI data acquisition
 - fMRI data preprocessing
 - Additional behavioral measures of memory performance
- [QUANTIFICATION AND STATISTICAL ANALYSIS](#)
 - General linear model (GLM)-based fMRI data analysis
 - Dynamic causal modeling
 - Prediction of memory performance from DCM parameters

SUPPLEMENTAL INFORMATION

Supplemental information can be found online at <https://doi.org/10.1016/j.isci.2023.107765>.

ACKNOWLEDGMENTS

The authors would like to thank Nadia Ay, Hannah Feldhoff, Larissa Fischer, Sophia Jauch, Lea Knopf, Matthias Raschick, Marc Roder, and Annika Schult for help with neuropsychological data collection and analysis, and Kerstin Möhring, Katja Neumann, Ilona Wiedenhöft, and Claus Tempelmann for assistance with MRI data acquisition. We further thank Emrah Düzel for helpful discussion during the planning stage and collaboration during data collection.

This study was supported by the State of Saxony-Anhalt and the European Regional Development Fund (Research Alliance “Autonomy in Old Age” to B.H.S.) and by the Deutsche Forschungsgemeinschaft (DFG CRC 1436, TP A05 to B.H.S., TP B01 to M.S., TP C01 to G.Z., and TP Z03 to A.M.; DFG RI 2964-1 to A.R.). The funding agencies had no role in the design or analysis of the study.

AUTHOR CONTRIBUTIONS

The authors confirm contribution to the study as follows: conceptualization: B.H.S., J.S., J.M.K., G.Z., and A.R.; investigation: A.A. and A.R.; methodology: B.H.S. and J.S.; formal analysis: B.H.S., J.S., and A.R.; project administration: B.H.S. and A.R.; software: B.H.S., J.S. and H.S.;

supervision: B.H.S.; visualization: B.H.S.; writing—original draft: B.H.S.; writing—editing: B.H.S., J.S., J.M.K., A.M., G.Z., M.S., and A.R.; and funding acquisition: B.H.S., A.M., G.Z., M.S., and A.R. All authors approved the final version of the manuscript.

DECLARATION OF INTERESTS

The authors declare no competing interests.

INCLUSION AND DIVERSITY

We support inclusive, diverse, and equitable conduct of research.

Received: January 5, 2023

Revised: June 30, 2023

Accepted: August 25, 2023

Published: August 29, 2023

REFERENCES

- Paller, K.A., Kutas, M., and Mayes, A.R. (1987). Neural correlates of encoding in an incidental learning paradigm. *Electroencephalogr. Clin. Neurophysiol.* 67, 360–371. [https://doi.org/10.1016/0013-4694\(87\)90124-6](https://doi.org/10.1016/0013-4694(87)90124-6).
- Brewer, J.B., Zhao, Z., Desmond, J.E., Glover, G.H., and Gabrieli, J.D. (1998). Making memories: brain activity that predicts how well visual experience will be remembered. *Science* 281, 1185–1187. <https://doi.org/10.1126/science.281.5380.1185>.
- Wagner, A.D., Schacter, D.L., Rotte, M., Koutstaal, W., Maril, A., Dale, A.M., Rosen, B.R., and Buckner, R.L. (1998). Building memories: remembering and forgetting of verbal experiences as predicted by brain activity. *Science* 281, 1188–1191. <https://doi.org/10.1126/science.281.5380.1188>.
- Kim, H. (2011). Neural activity that predicts subsequent memory and forgetting: a meta-analysis of 74 fMRI studies. *Neuroimage* 54, 2446–2461. <https://doi.org/10.1016/j.neuroimage.2010.09.045>.
- Maillet, D., and Rajah, M.N. (2014). Age-related differences in brain activity in the subsequent memory paradigm: a meta-analysis. *Neurosci. Biobehav. Rev.* 45, 246–257. <https://doi.org/10.1016/j.neubiorev.2014.06.006>.
- Nyberg, L. (2017). Functional brain imaging of episodic memory decline in ageing. *J. Intern. Med.* 281, 65–74. <https://doi.org/10.1111/joim.12533>.
- Roscom, A.M., Good, C.D., Frackowiak, R.S.J., and Rugg, M.D. (2003). Age effects on the neural correlates of successful memory encoding. *Brain* 126, 213–229. <https://doi.org/10.1093/brain/awg020>.
- Düzel, E., Schütze, H., Yonelinas, A.P., and Heinze, H.J. (2011). Functional phenotyping of successful aging in long-term memory: Preserved performance in the absence of neural compensation. *Hippocampus* 21, 803–814. <https://doi.org/10.1002/hipo.20834>.
- Grady, C.L., Springer, M.V., Hongwanishkul, D., McIntosh, A.R., and Winocur, G. (2006). Age-related changes in brain activity across the adult lifespan. *J. Cognit. Neurosci.* 18, 227–241. <https://doi.org/10.1162/08992906775783705>.
- Hafkemeijer, A., van der Grond, J., and Rombouts, S.A.R.B. (2012). Imaging the default mode network in aging and dementia. *Biochim. Biophys. Acta* 1822, 431–441. <https://doi.org/10.1016/j.bbdis.2011.07.008>.
- Malagurski, B., Liem, F., Oschwald, J., Méritat, S., and Jäncke, L. (2020). Functional dedifferentiation of associative resting state networks in older adults - A longitudinal study. *Neuroimage* 214, 116680. <https://doi.org/10.1016/j.neuroimage.2020.116680>.
- Deshpande, G., Zhao, X., and Robinson, J. (2022). Functional parcellation of the hippocampus based on its layer-specific connectivity with default mode and dorsal attention networks. *Neuroimage* 254, 119078. <https://doi.org/10.1016/j.neuroimage.2022.119078>.
- Beason-Held, L.L., Shafer, A.T., Goh, J.O., Landman, B.A., Davatzikos, C., Viscomi, B., Ash, J., Kitner-Triolo, M., Ferrucci, L., and Resnick, S.M. (2021). Hippocampal activation and connectivity in the aging brain. *Brain Imaging Behav.* 15, 711–726. <https://doi.org/10.1007/s11682-020-00279-6>.
- Cohen, M.X. (2011). Hippocampal-prefrontal connectivity predicts midfrontal oscillations and long-term memory performance. *Curr. Biol.* 21, 1900–1905. <https://doi.org/10.1016/j.cub.2011.09.036>.
- Cooper, R.A., and Ritchey, M. (2019). Cortico-hippocampal network connections support the multidimensional quality of episodic memory. *Elife* 8, e45591. <https://doi.org/10.7554/eLife.45591>.
- Fuentemilla, L., Càmarà, E., Münte, T.F., Krämer, U.M., Cunillera, T., Marco-Pallarés, J., Tempelmann, C., and Rodríguez-Fornells, A. (2009). Individual differences in true and false memory retrieval are related to white matter brain microstructure. *J. Neurosci.* 29, 8698–8703. <https://doi.org/10.1523/jneurosci.5270-08.2009>.
- Schott, B.H., Niklas, C., Kaufmann, J., Bodammer, N.C., Machts, J., Schütze, H., and Düzel, E. (2011). Fiber density between rhinal cortex and activated ventrolateral prefrontal regions predicts episodic memory performance in humans. *Proc. Natl. Acad. Sci. USA* 108, 5408–5413. <https://doi.org/10.1073/pnas.1013287108>.
- Schott, B.H., Wüstenberg, T., Wimber, M., Fenker, D.B., Zierhut, K.C., Seidenbecher, C.I., Heinze, H.J., Walter, H., Düzel, E., and Richardson-Klavehn, A. (2013). The relationship between level of processing and hippocampal-cortical functional connectivity during episodic memory formation in humans. *Hum. Brain Mapp.* 34, 407–424. <https://doi.org/10.1002/hbm.21435>.
- Stark, S.M., Frithsen, A., and Stark, C.E.L. (2021). Age-related alterations in functional connectivity along the longitudinal axis of the hippocampus and its subfields. *Hippocampus* 31, 11–27. <https://doi.org/10.1002/hipo.23259>.
- Penny, W.D., Stephan, K.E., Mechelli, A., and Friston, K.J. (2004). Modelling functional integration: a comparison of structural equation and dynamic causal models. *Neuroimage* 23 (Suppl 1), S264–S274. <https://doi.org/10.1016/j.neuroimage.2004.07.041>.
- Nyberg, L., Andersson, M., Lundquist, A., Salami, A., and Wåhlin, A. (2019). Frontal Contribution to Hippocampal Hyperactivity During Memory Encoding in Aging. *Front. Mol. Neurosci.* 12, 229. <https://doi.org/10.3389/fnmol.2019.00229>.
- Diersch, N., Valdes-Herrera, J.P., Tempelmann, C., and Wolbers, T. (2021). Increased Hippocampal Excitability and Altered Learning Dynamics Mediate Cognitive Mapping Deficits in Human Aging. *J. Neurosci.* 41, 3204–3221. <https://doi.org/10.1523/jneurosci.0528-20.2021>.
- Soch, J., Richter, A., Schütze, H., Kizilirmak, J.M., Assmann, A., Knopf, L., Raschick, M., Schult, A., Maass, A., Ziegler, G., et al. (2021). Bayesian model selection favors parametric over categorical fMRI subsequent memory models in young and older adults. *Neuroimage* 230, 117820. <https://doi.org/10.1016/j.neuroimage.2021.117820>.
- Kizilirmak, J.M., Soch, J., Schütze, H., Düzel, E., Feldhoff, H., Fischer, L., Knopf, L., Maass, A., Raschick, M., Schult, A., et al. (2023). The relationship between resting-state amplitude fluctuations and memory-related deactivations of the default mode network in young and older adults. *Hum. Brain Mapp.* 44, 3586–3609. <https://doi.org/10.1002/hbm.26299>.
- Zeidman, P., Jafarian, A., Corbin, N., Seghier, M.L., Razi, A., Price, C.J., and Friston, K.J. (2019). A guide to group effective connectivity analysis, part 1: First level analysis with DCM for fMRI. *Neuroimage* 200, 174–190. <https://doi.org/10.1016/j.neuroimage.2019.06.031>.

26. Zeidman, P., Jafarian, A., Seghier, M.L., Litvak, V., Cagnan, H., Price, C.J., and Friston, K.J. (2019). A guide to group effective connectivity analysis, part 2: Second level analysis with PEB. *Neuroimage* 200, 12–25. <https://doi.org/10.1016/j.neuroimage.2019.06.032>.
27. Aminoff, E.M., Kveraga, K., and Bar, M. (2013). The role of the parahippocampal cortex in cognition. *Trends Cognit. Sci.* 17, 379–390. <https://doi.org/10.1016/j.tics.2013.06.009>.
28. Gilmore, A.W., Nelson, S.M., and McDermott, K.B. (2015). A parietal memory network revealed by multiple MRI methods. *Trends Cognit. Sci.* 19, 534–543. <https://doi.org/10.1016/j.tics.2015.07.004>.
29. Uncapher, M.R., and Wagner, A.D. (2009). Posterior parietal cortex and episodic encoding: insights from fMRI subsequent memory effects and dual-attention theory. *Neurobiol. Learn. Mem.* 91, 139–154. <https://doi.org/10.1016/j.nlm.2008.10.011>.
30. Soch, J., Richter, A., Schütze, H., Kizilirmak, J.M., Assmann, A., Behnisch, G., Feldhoff, H., Fischer, L., Heil, J., Knopf, L., et al. (2021). A comprehensive score reflecting memory-related fMRI activations and deactivations as potential biomarker for neurocognitive aging. *Hum. Brain Mapp.* 42, 4478–4496. <https://doi.org/10.1002/hbm.25559>.
31. Bunzeck, N., Schütze, H., and Düzel, E. (2006). Category-specific organization of prefrontal response-facilitation during priming. *Neuropsychologia* 44, 1765–1776. <https://doi.org/10.1016/j.neuropsychologia.2006.03.019>.
32. Stephan, K.E., Marshall, J.C., Penny, W.D., Friston, K.J., and Fink, G.R. (2007). Interhemispheric integration of visual processing during task-driven lateralization. *J. Neurosci.* 27, 3512–3522. <https://doi.org/10.1523/jneurosci.4766-06.2007>.
33. Fujii, T., Tanabe, H.C., Kochiyama, T., and Sadato, N. (2009). An investigation of cross-modal plasticity of effective connectivity in the blind by dynamic causal modeling of functional MRI data. *Neurosci. Res.* 65, 175–186. <https://doi.org/10.1016/j.neures.2009.06.014>.
34. Yang, Y., Zhong, N., Friston, K., Imamura, K., Lu, S., Li, M., Zhou, H., Wang, H., Li, K., and Hu, B. (2017). The functional architectures of addition and subtraction: Network discovery using fMRI and DCM. *Hum. Brain Mapp.* 38, 3210–3225. <https://doi.org/10.1002/hbm.23585>.
35. Schwarzkopf, D.S., De Haas, B., and Rees, G. (2012). Better ways to improve standards in brain-behavior correlation analysis. *Front. Hum. Neurosci.* 6, 200. <https://doi.org/10.3389/fnhum.2012.00200>.
36. Wetzels, R., and Wagenmakers, E.J. (2012). A default Bayesian hypothesis test for correlations and partial correlations. *Psychon. Bull. Rev.* 19, 1057–1064. <https://doi.org/10.3758/s13423-012-0295-x>.
37. Helmstaedter, C. (2001). VLMT: Verbaler Lern- und Merkfähigkeitstest (Beltz Test).
38. Härting, C., Markowitsch, H.-J., Neufeld, H., Calabrese, P., Deisinger, K., and Kessler, J. (2000). *Wechsler Memory Scale, Revised Edition, German Edition. Manual (Huber)*.
39. Köhler, S., Crane, J., and Milner, B. (2002). Differential contributions of the parahippocampal place area and the anterior hippocampus to human memory for scenes. *Hippocampus* 12, 718–723. <https://doi.org/10.1002/hipo.10077>.
40. Kremers, N.A.W., Deuker, L., Kranz, T.A., Oehrn, C., Fell, J., and Axmacher, N. (2014). Hippocampal control of repetition effects for associative stimuli. *Hippocampus* 24, 892–902. <https://doi.org/10.1002/hipo.22278>.
41. Dennis, N.A., Hayes, S.M., Prince, S.E., Madden, D.J., Huettel, S.A., and Cabeza, R. (2008). Effects of aging on the neural correlates of successful item and source memory encoding. *J. Exp. Psychol. Learn. Mem. Cogn.* 34, 791–808. <https://doi.org/10.1037/0278-7393.34.4.791>.
42. Eichenbaum, H., Yonelinas, A.P., and Ranganath, C. (2007). The medial temporal lobe and recognition memory. *Annu. Rev. Neurosci.* 30, 123–152. <https://doi.org/10.1146/annurev.neuro.30.051606.094328>.
43. Kinnavane, L., Amin, E., Horne, M., and Aggleton, J.P. (2014). Mapping parahippocampal systems for recognition and recency memory in the absence of the rat hippocampus. *Eur. J. Neurosci.* 40, 3720–3734. <https://doi.org/10.1111/ejn.12740>.
44. Olarte-Sánchez, C.M., Kinnavane, L., Amin, E., and Aggleton, J.P. (2014). Contrasting networks for recognition memory and recency memory revealed by immediately gene imaging in the rat. *Behav. Neurosci.* 128, 504–522. <https://doi.org/10.1037/a0037055>.
45. Marks, W.D., Yamamoto, N., and Kitamura, T. (2021). Complementary roles of differential medial entorhinal cortex inputs to the hippocampus for the formation and integration of temporal and contextual memory (Systems Neuroscience). *Eur. J. Neurosci.* 54, 6762–6779. <https://doi.org/10.1111/ejn.14737>.
46. Epstein, R.A., and Baker, C.I. (2019). Scene Perception in the Human Brain. *Annu. Rev. Vis. Sci.* 5, 373–397. <https://doi.org/10.1146/annurev-vision-091718-014809>.
47. Ranganath, C., and Rainer, G. (2003). Neural mechanisms for detecting and remembering novel events. *Nat. Rev. Neurosci.* 4, 193–202. <https://doi.org/10.1038/nrn1052>.
48. Kumaran, D., and Maguire, E.A. (2007). Match mismatch processes underlie human hippocampal responses to associative novelty. *J. Neurosci.* 27, 8517–8524. <https://doi.org/10.1523/jneurosci.1677-07.2007>.
49. Düzel, E., Ziegler, G., Berron, D., Maass, A., Schütze, H., Cardenas-Blanco, A., Glanz, W., Metzger, C., Dobisch, L., Reuter, M., et al. (2022). Amyloid pathology but not APOE ε4 status is permissive for tau-related hippocampal dysfunction. *Brain* 145, 1473–1485. <https://doi.org/10.1093/brain/awab405>.
50. Billette, O.V., Ziegler, G., Aruci, M., Schütze, H., Kizilirmak, J.M., Richter, A., Altenstein, S., Bartels, C., Brosseron, F., Cardenas-Blanco, A., et al. (2022). Novelty-Related fMRI Responses of Precuneus and Medial Temporal Regions in Individuals at Risk for Alzheimer Disease. *Neurology* 99, e775–e788. <https://doi.org/10.1212/wnl.0000000000200667>.
51. Salami, A., Wählin, A., Kaboodvand, N., Lundquist, A., and Nyberg, L. (2016). Longitudinal Evidence for Dissociation of Anterior and Posterior MTL Resting-State Connectivity in Aging: Links to Perfusion and Memory. *Cerebr. Cortex* 26, 3953–3963. <https://doi.org/10.1093/cercor/bhw233>.
52. Buckner, R.L., Andrews-Hanna, J.R., and Schacter, D.L. (2008). The brain's default network: anatomy, function, and relevance to disease. *Ann. N. Y. Acad. Sci.* 1124, 1–38. <https://doi.org/10.1196/annals.1440.011>.
53. Qin, P., Liu, Y., Shi, J., Wang, Y., Duncan, N., Gong, Q., Weng, X., and Northoff, G. (2012). Dissociation between anterior and posterior cortical regions during self-specificity and familiarity: a combined fMRI-meta-analytic study. *Hum. Brain Mapp.* 33, 154–164. <https://doi.org/10.1002/hbm.21201>.
54. Ranganath, C., and Ritchey, M. (2012). Two cortical systems for memory-guided behaviour. *Nat. Rev. Neurosci.* 13, 713–726. <https://doi.org/10.1038/nrn3338>.
55. Cabeza, R., Albert, M., Belleville, S., Craik, F.I.M., Duarte, A., Grady, C.L., Lindenberger, U., Nyberg, L., Park, D.C., Reuter-Lorenz, P.A., et al. (2018). Maintenance, reserve and compensation: the cognitive neuroscience of healthy ageing. *Nat. Rev. Neurosci.* 19, 701–710. <https://doi.org/10.1038/s41583-018-0068-2>.
56. Soch, J., Richter, A., Kizilirmak, J.M., Schütze, H., Feldhoff, H., Fischer, L., Knopf, L., Raschick, M., Schult, A., Düzel, E., and Schott, B.H. (2022). Structural and functional MRI data differentially predict chronological age and behavioral memory performance. *eNeuro* 9, ENEURO.0212-22.2022. <https://doi.org/10.1523/ENEURO.0212-22.2022>.
57. Richter, A., Soch, J., Kizilirmak, J.M., Fischer, L., Schütze, H., Assmann, A., Behnisch, G., Feldhoff, H., Knopf, L., Raschick, M., et al. (2023). Single-value scores of memory-related brain activity reflect dissociable neuropsychological and anatomical signatures of neurocognitive aging. *Hum. Brain Mapp.* 44, 3283–3301. <https://doi.org/10.1002/hbm.26281>.
58. Li, Y., Cheng, J.X., and Yu, J. (2022). Episodic memory updating among older adults: moderating role of prior knowledge. *Memory* 30, 1240–1247. <https://doi.org/10.1080/09658211.2022.2099901>.
59. Chen, X., Varghese, L., and Jagust, W.J. (2022). A Double-Edged Sword: The Role of Prior Knowledge in Memory Aging. *Front. Aging Neurosci.* 14, 874767. <https://doi.org/10.3389/fnagi.2022.874767>.
60. Kizilirmak, J.M., Fischer, L., Krause, J., Soch, J., Richter, A., and Schott, B.H. (2021). Learning by Insight-Like Sudden Comprehension as a Potential Strategy to Improve Memory Encoding in Older Adults. *Front. Aging Neurosci.* 13, 661346. <https://doi.org/10.3389/fnagi.2021.661346>.
61. Sperling, R.A., Laviolette, P.S., O'Keefe, K., O'Brien, J., Rentz, D.M., Pihlajamäki, M., Marshall, G., Hyman, B.T., Selkoe, D.J., Hedden, T., et al. (2009). Amyloid deposition is associated with impaired default network function in older persons without dementia. *Neuron* 63, 178–188. <https://doi.org/10.1016/j.neuron.2009.07.003>.
62. Sambataro, F., Murty, V.P., Callicott, J.H., Tan, H.Y., Das, S., Weinberger, D.R., and Mattay, V.S. (2010). Age-related alterations in default mode network: impact on working memory performance. *Neurobiol. Aging* 31, 839–852. <https://doi.org/10.1016/j.neurobiolaging.2008.05.022>.
63. Knights, E., Morcom, A.M., and Henson, R.N. (2021). Does Hemispheric Asymmetry Reduction in Older Adults in Motor Cortex Reflect Compensation? *J. Neurosci.* 41, 9361–9373. <https://doi.org/10.1523/jneurosci.1111-21.2021>.

64. Vilberg, K.L., and Rugg, M.D. (2008). Memory retrieval and the parietal cortex: a review of evidence from a dual-process perspective. *Neuropsychologia* 46, 1787–1799. <https://doi.org/10.1016/j.neuropsychologia.2008.01.004>.
65. Kernbach, J.M., Yeo, B.T.T., Smallwood, J., Margulies, D.S., Thiebaut de Schotten, M., Walter, H., Sabuncu, M.R., Holmes, A.J., Gramfort, A., Varoquaux, G., et al. (2018). Subspecialization within default mode nodes characterized in 10,000 UK Biobank participants. *Proc. Natl. Acad. Sci. USA* 115, 12295–12300. <https://doi.org/10.1073/pnas.1804876115>.
66. Utevsky, A.V., Smith, D.V., and Huettel, S.A. (2014). Precuneus is a functional core of the default-mode network. *J. Neurosci.* 34, 932–940. <https://doi.org/10.1523/Jneurosci.4227-13.2014>.
67. Lyu, D., Pappas, I., Menon, D.K., and Stamatakis, E.A. (2021). A Precuneal Causal Loop Mediates External and Internal Information Integration in the Human Brain. *J. Neurosci.* 41, 9944–9956. <https://doi.org/10.1523/jneurosci.0647-21.2021>.
68. Brodt, S., Pöhlchen, D., Flanagan, V.L., Glasauer, S., Gais, S., and Schönauer, M. (2016). Rapid and independent memory formation in the parietal cortex. *Proc. Natl. Acad. Sci. USA* 113, 13251–13256. <https://doi.org/10.1073/pnas.1605719113>.
69. Brodt, S., Gais, S., Beck, J., Erb, M., Scheffler, K., and Schönauer, M. (2018). Fast track to the neocortex: A memory engram in the posterior parietal cortex. *Science* 362, 1045–1048. <https://doi.org/10.1126/science.aau2528>.
70. Schott, B.H., Wüstenberg, T., Lücke, E., Pohl, I.M., Richter, A., Seidenbecher, C.I., Pollmann, S., Kizilirmak, J.M., and Richardson-Klavehn, A. (2019). Gradual acquisition of visuospatial associative memory representations via the dorsal precuneus. *Hum. Brain Mapp.* 40, 1554–1570. <https://doi.org/10.1002/hbm.24467>.
71. Henke, K. (2010). A model for memory systems based on processing modes rather than consciousness. *Nat. Rev. Neurosci.* 11, 523–532. <https://doi.org/10.1038/nrn2850>.
72. Brodt, S., and Gais, S. (2021). Memory Engrams in the Neocortex. *Neuroscientist* 27, 427–444. <https://doi.org/10.1177/1073858420941528>.
73. van Kesteren, M.T.R., Ruiter, D.J., Fernández, G., and Henson, R.N. (2012). How schema and novelty augment memory formation. *Trends Neurosci.* 35, 211–219. <https://doi.org/10.1016/j.tins.2012.02.001>.
74. Renoult, L., Irish, M., Moscovitch, M., and Rugg, M.D. (2019). From Knowing to Remembering: The Semantic-Episodic Distinction. *Trends Cognit. Sci.* 23, 1041–1057. <https://doi.org/10.1016/j.tics.2019.09.008>.
75. Mills-Finnerty, C. (2021). Five best practices for fMRI research: Towards a biologically grounded understanding of mental phenomena. *J. Rep. Neurosci.* 2, 1517. <https://doi.org/10.31885/jrn.2.2021.1517>.
76. Bossier, H., Roels, S.P., Seurinck, R., Banaschewski, T., Barker, G.J., Bokde, A.L.W., Quinlan, E.B., Desrivieres, S., Flor, H., Grigis, A., et al. (2020). The empirical replicability of task-based fMRI as a function of sample size. *Neuroimage* 212, 116601. <https://doi.org/10.1016/j.neuroimage.2020.116601>.
77. Kampa, M., Schick, A., Sebastian, A., Wessa, M., Tüscher, O., Kalisch, R., and Yuen, K. (2020). Replication of fMRI group activations in the neuroimaging battery for the Mainz Resilience Project (MARP). *Neuroimage* 204, 116223. <https://doi.org/10.1016/j.neuroimage.2019.116223>.
78. Almeida, J.R.C.d., Kronhaus, D.M., Sibille, E.L., Langenecker, S.A., Versace, A., Labarbara, E.J., and Phillips, M.L. (2011). Abnormal left-sided orbitomedial prefrontal cortical-amygdala connectivity during happy and fear face processing: a potential neural mechanism of female MDD. *Front. Psychiatr.* 2, 69. <https://doi.org/10.3389/fpsyt.2011.00069>.
79. Tzvi, E., Zimmermann, C., Bey, R., Münte, T.F., Nitschke, M., and Krämer, U.M. (2017). Cerebellar degeneration affects cortico-cortical connectivity in motor learning networks. *Neuroimage. Clin.* 16, 66–78. <https://doi.org/10.1016/j.nicl.2017.07.012>.
80. Wroblewski, A., He, Y., and Straube, B. (2020). Dynamic Causal Modeling suggests impaired effective connectivity in patients with schizophrenia spectrum disorders during gesture-speech integration. *Schizophr. Res.* 216, 175–183. <https://doi.org/10.1016/j.schres.2019.12.005>.
81. Sjuls, G.S., and Specht, K. (2022). Variability in Resting-State Functional Magnetic Resonance Imaging: The Effect of Body Mass, Blood Pressure, Hematocrit, and Glycated Hemoglobin on Hemodynamic and Neuronal Parameters. *Brain Connect.* 12, 870–882. <https://doi.org/10.1089/brain.2021.0125>.
82. Snyder, A.D., Ma, L., Steinberg, J.L., Woisard, K., and Moeller, F.G. (2021). Dynamic Causal Modeling Self-Connectivity Findings in the Functional Magnetic Resonance Imaging Neuropsychiatric Literature. *Front. Neurosci.* 15, 636273. <https://doi.org/10.3389/fnins.2021.636273>.
83. Nikolakopoulos, S., and Ntzoufras, I. (2021). Meta Analysis of Bayes Factors. Preprint at arXiv. <https://doi.org/10.48550/arXiv.2103.13236>.
84. Goodman, S.N. (2016). STATISTICS. Aligning statistical and scientific reasoning. *Science* 352, 1180–1181. <https://doi.org/10.1126/science.aaf5406>.
85. Rouder, J.N., and Morey, R.D. (2011). A Bayes factor meta-analysis of Bem's ESP claim. *Psychon. Bull. Rev.* 18, 682–689. <https://doi.org/10.3758/s13423-011-0088-7>.
86. Naze, S., Hearne, L.J., Roberts, J.A., Sanz-Leon, P., Burgher, B., Hall, C., Sonkusare, S., Nott, Z., Marcus, L., Savage, E., et al. (2023). Mechanisms of imbalanced frontostriatal functional connectivity in obsessive-compulsive disorder. *Brain* 146, 1322–1327. <https://doi.org/10.1093/brain/awac425>.
87. Lohmann, G., Erfurth, K., Müller, K., and Turner, R. (2012). Critical comments on dynamic causal modelling. *Neuroimage* 59, 2322–2329. <https://doi.org/10.1016/j.neuroimage.2011.09.025>.
88. Daunizeau, J., David, O., and Stephan, K.E. (2011). Dynamic causal modelling: a critical review of the biophysical and statistical foundations. *Neuroimage* 58, 312–322. <https://doi.org/10.1016/j.neuroimage.2009.11.062>.
89. Havlicek, M., Roebroeck, A., Friston, K., Gardumi, A., Ivanov, D., and Uludag, K. (2015). Physiologically informed dynamic causal modeling of fMRI data. *Neuroimage* 122, 355–372. <https://doi.org/10.1016/j.neuroimage.2015.07.078>.
90. Havlicek, M., Ivanov, D., Roebroeck, A., and Uludag, K. (2017). Determining Excitatory and Inhibitory Neuronal Activity from Multimodal fMRI Data Using a Generative Hemodynamic Model. *Front. Neurosci.* 11, 616. <https://doi.org/10.3389/fnins.2017.00616>.
91. Uludag, K. (2023). Physiological Modeling of the BOLD signal and Implications for Effective Connectivity: a primer. *Neuroimage* 20249. <https://doi.org/10.1016/j.neuroimage.2023.120249>.
92. Friston, K.J., Preller, K.H., Mathys, C., Cagnan, H., Heinzle, J., Razi, A., and Zeidman, P. (2019). Dynamic causal modelling revisited. *Neuroimage* 199, 730–744. <https://doi.org/10.1016/j.neuroimage.2017.02.045>.
93. Cansino, S., Trejo-Morales, P., Estrada-Manilla, C., Pasaye-Alcaraz, E.H., Aguilar-Castañeda, E., Salgado-Lujambio, P., and Sosa-Ortiz, A.L. (2017). Effective connectivity during successful and unsuccessful recollection in young and old adults. *Neuropsychologia* 103, 168–182. <https://doi.org/10.1016/j.neuropsychologia.2017.07.016>.
94. Legon, W., Punzell, S., Dowlati, E., Adams, S.E., Stiles, A.B., and Moran, R.J. (2016). Altered Prefrontal Excitation/Inhibition Balance and Prefrontal Output: Markers of Aging in Human Memory Networks. *Cerebr. Cortex* 26, 4315–4326. <https://doi.org/10.1093/cercor/bhv200>.
95. Nordin, K., Herlitz, A., Larsson, E.-M., and Söderlund, H. (2017). Overlapping effects of age on associative memory and the anterior hippocampus from middle to older age. *Behav. Brain Res.* 317, 350–359.
96. Damoiseaux, J.S., Viviano, R.P., Yuan, P., and Raz, N. (2016). Differential effect of age on posterior and anterior hippocampal functional connectivity. *Neuroimage* 133, 468–476.
97. Zweynert, S., Pade, J.P., Wüstenberg, T., Sterzer, P., Walter, H., Seidenbecher, C.I., Richardson-Klavehn, A., Düzel, E., and Schott, B.H. (2011). Motivational salience modulates hippocampal repetition suppression and functional connectivity in humans. *Front. Hum. Neurosci.* 5, 144. <https://doi.org/10.3389/fnhum.2011.00144>.
98. Sheehan, D.V., Lecrubier, Y., Sheehan, K.H., Amorim, P., Janavs, J., Weiller, E., Hergueta, T., Baker, R., and Dunbar, G.C. (1998). The Mini-International Neuropsychiatric Interview (M.I.N.I.): the development and validation of a structured diagnostic psychiatric interview for DSM-IV and ICD-10. *J. Clin. Psychiatry* 59 (Suppl 20), 22–33.
99. Ackenheil, M., Stotz, G., Dietz-Bauer, R., Vossen, A., Dietz, R., Vossen-Wellmann, A., and Vossen, J.A. (1999). Mini International Neuropsychiatric Interview. German Version 5.0.0, DSM-IV (Psychiatrische Universitätsklinik München).
100. Assmann, A., Richter, A., Schütze, H., Soch, J., Barman, A., Behnisch, G., Knopf, L., Raschick, M., Schult, A., Wüstenberg, T., et al. (2021). Neurocan genome-wide psychiatric risk variant affects explicit memory performance and hippocampal function in healthy humans. *Eur. J. Neurosci.* 53, 3942–3959. <https://doi.org/10.1111/ejn.14872>.
101. World Medical Association (2013). World Medical Association Declaration of

- Helsinki: ethical principles for medical research involving human subjects. *JAMA* 310, 2191–2194. <https://doi.org/10.1001/jama.2013.281053>.
102. Barman, A., Assmann, A., Richter, S., Soch, J., Schütze, H., Wüstenberg, T., Deibele, A., Klein, M., Richter, A., Behnisch, G., et al. (2014). Genetic variation of the RASGRF1 regulatory region affects human hippocampus-dependent memory. *Front. Hum. Neurosci.* 8, 260. <https://doi.org/10.3389/fnhum.2014.00260>.
 103. Schott, B.H., Assmann, A., Schmierer, P., Soch, J., Erk, S., Garbusow, M., Mohnke, S., Pöhlend, L., Romanczuk-Seiferth, N., Barman, A., et al. (2014). Epistatic interaction of genetic depression risk variants in the human subgenual cingulate cortex during memory encoding. *Transl. Psychiatry* 4, e372. <https://doi.org/10.1038/tp.2014.10>.
 104. Bainbridge, W.A., Berron, D., Schütze, H., Cardenas-Blanco, A., Metzger, C., Dobisch, L., Bittner, D., Glanz, W., Spottke, A., Rudolph, J., et al. (2019). Memorability of photographs in subjective cognitive decline and mild cognitive impairment: Implications for cognitive assessment. *Alzheimers Dement.* 11, 610–618. <https://doi.org/10.1016/j.dadm.2019.07.005>.
 105. Hinrichs, H., Scholz, M., Tempelmann, C., Woldorff, M.G., Dale, A.M., and Heinze, H.J. (2000). Deconvolution of event-related fMRI responses in fast-rate experimental designs: tracking amplitude variations. *J. Cognit. Neurosci.* 12 (Suppl 2), 76–89. <https://doi.org/10.1162/089892900564082>.
 106. Düzel, E., Berron, D., Schütze, H., Cardenas-Blanco, A., Metzger, C., Betts, M., Ziegler, G., Chen, Y., Dobisch, L., Bittner, D., et al. (2018). CSF total tau levels are associated with hippocampal novelty irrespective of hippocampal volume. *Alzheimers Dement.* 10, 782–790. <https://doi.org/10.1016/j.dadm.2018.10.003>.
 107. Jessen, F., Spottke, A., Boecker, H., Brosse, F., Buerger, K., Catak, C., Fließbach, K., Franke, C., Fuentes, M., Heneka, M.T., et al. (2018). Design and first baseline data of the DZNE multicenter observational study on predementia Alzheimer's disease (DELCODE). *Alzheimer's Res. Ther.* 10, 15. <https://doi.org/10.1186/s13195-017-0314-2>.
 108. Raschick, M., Richter, A., Fischer, L., Knopf, L., Schult, A., Yakupov, R., Behnisch, G., Guttek, K., Düzel, E., Dunay, I.R., et al. (2023). Plasma concentrations of anti-inflammatory cytokine TGF- β are associated with hippocampal structure related to explicit memory performance in older adults. *J. Neural. Transm.* 130, 989–1002. <https://doi.org/10.1007/s00702-023-02638-1>.
 109. Tzourio-Mazoyer, N., Landeau, B., Papathanassiou, D., Crivello, F., Etard, O., Delcroix, N., Mazoyer, B., and Joliot, M. (2002). Automated anatomical labeling of activations in SPM using a macroscopic anatomical parcellation of the MNI MRI single-subject brain. *Neuroimage* 15, 273–289. <https://doi.org/10.1006/nimg.2001.0978>.
 110. Epstein, R.A. (2008). Parahippocampal and retrosplenial contributions to human spatial navigation. *Trends Cognit. Sci.* 12, 388–396. <https://doi.org/10.1016/j.tics.2008.07.004>.
 111. Seghier, M.L., Zeidman, P., Neufeld, N.H., Leff, A.P., and Price, C.J. (2010). Identifying abnormal connectivity in patients using dynamic causal modeling of fMRI responses. *Front. Syst. Neurosci.* 4, 142. <https://doi.org/10.3389/fnsys.2010.00142>.
 112. Bencivenga, F., Sulpizio, V., Tullo, M.G., and Galati, G. (2021). Assessing the effective connectivity of premotor areas during real vs imagined grasping: a DCM-PEB approach. *Neuroimage* 230, 117806. <https://doi.org/10.1016/j.neuroimage.2021.117806>.
 113. Sacu, S., Wackerhagen, C., Erk, S., Romanczuk-Seiferth, N., Schwarz, K., Schweiger, J.I., Tost, H., Meyer-Lindenberg, A., Heinz, A., Razi, A., and Walter, H. (2022). Effective connectivity during face processing in major depression - distinguishing markers of pathology, risk, and resilience. *Psychol. Med.* 53, 1–13. <https://doi.org/10.1017/S0033291722000824>.
 114. Kiebel, S.J., Klöppel, S., Weiskopf, N., and Friston, K.J. (2007). Dynamic causal modeling: a generative model of slice timing in fMRI. *Neuroimage* 34, 1487–1496. <https://doi.org/10.1016/j.neuroimage.2006.10.026>.
 115. Seghier, M.L., Josse, G., Leff, A.P., and Price, C.J. (2011). Lateralization is predicted by reduced coupling from the left to right prefrontal cortex during semantic decisions on written words. *Cerebr. Cortex* 21, 1519–1531. <https://doi.org/10.1093/cercor/bhq203>.
 116. Friston, K.J., Litvak, V., Oswal, A., Razi, A., Stephan, K.E., van Wijk, B.C.M., Ziegler, G., and Zeidman, P. (2016). Bayesian model reduction and empirical Bayes for group (DCM) studies. *Neuroimage* 128, 413–431. <https://doi.org/10.1016/j.neuroimage.2015.11.015>.
 117. Friston, K., Mattout, J., Trujillo-Barreto, N., Ashburner, J., and Penny, W. (2007). Variational free energy and the Laplace approximation. *Neuroimage* 34, 220–234. <https://doi.org/10.1016/j.neuroimage.2006.08.035>.
 118. Dijkstra, N., Zeidman, P., Ondobaka, S., van Gerven, M.A.J., and Friston, K. (2017). Distinct Top-down and Bottom-up Brain Connectivity During Visual Perception and Imagery. *Sci. Rep.* 7, 5677. <https://doi.org/10.1038/s41598-017-05888-8>.
 119. Friston, K., and Penny, W. (2011). Post hoc Bayesian model selection. *Neuroimage* 56, 2089–2099. <https://doi.org/10.1016/j.neuroimage.2011.03.062>.
 120. Penny, W.D., Stephan, K.E., Daunizeau, J., Rosa, M.J., Friston, K.J., Schofield, T.M., and Leff, A.P. (2010). Comparing families of dynamic causal models. *PLoS Comput. Biol.* 6, e1000709. <https://doi.org/10.1371/journal.pcbi.1000709>.
 121. Macmillan, N.A., and Creelman, C.D. (1991). *Detection Theory: A User's Guide* (Cambridge University Press).
 122. Kerkelberg, B. (2022). *BayesFactor: Release 2022*.
 123. Yarkoni, T. (2009). Big Correlations in Little Studies: Inflated fMRI Correlations Reflect Low Statistical Power-Commentary on Vul et al. (2009). *Perspect. Psychol. Sci.* 4, 294–298. <https://doi.org/10.1111/j.1745-6924.2009.01127.x>.
 124. Rousselet, G.A., and Pernet, C.R. (2012). Improving standards in brain-behavior correlation analyses. *Front. Hum. Neurosci.* 6, 119. <https://doi.org/10.3389/fnhum.2012.00119>.
 125. Zellner, A. (1986). On assessing prior distributions and Bayesian regression analysis with g-prior distributions. In *Bayesian Inference and Decision Techniques: Essays in Honor of Bruno de Finetti*, P.K. Goel and A. Zellner, eds. (Elsevier), pp. 233–243.
 126. Liang, F., Paulo, R., Molina, G., Clyde, M.A., and Berger, J.O. (2008). Mixtures of g priors for Bayesian variable selection. *J. Am. Stat. Assoc.* 103, 410–423.

STAR★METHODS

KEY RESOURCES TABLE

REAGENT or RESOURCE	SOURCE	IDENTIFIER
Deposited data		
Collated single subjects' DCMs and templates (GCM_*.mat)	Björn H. Schott via OSF	https://osf.io/ktqy6/
Group level fMRI contrasts	NeuroVault	https://osf.io/ktqy6/
ROI masks (PPA probabilistic ROI and anatomical masks for all ROIs)	Zweynert et al., 2011 ⁹⁷ /Björn H. Schott via OSF	https://osf.io/ktqy6/
Single subjects' raw fMRI data (Autonomy in Old Age)	Leibniz Institute for Neurobiology (LIN)	N/A
Software and algorithms		
Matlab R2018b	MathWorks, Natick, MA	https://de.mathworks.com/products/matlab.html
Statistical Parametric Mapping (SPM12, v7771), including DCM 12.5	Wellcome Trust Centre for Neuroimaging	https://www.fil.ion.ucl.ac.uk/spm/
Parametric first-level fMRI data analysis described by Soch et al., 2021 ²³	Joram Soch via GitHub	https://github.com/JoramSoch/FADE_BMS
Matlab scripts for ROI selection, DCM batch analysis, and brain-behavior correlations	Björn H. Schott via GitHub	https://github.com/bhschott/DCM_MemoryEncoding
WFU Pickatlas	Wake Forest University	https://www.nitrc.org/projects/wfu_pickatlas/
Shepherd's Pi Correlation	Sam Schwarzkopf	https://www.frontiersin.org/articles/10.3389/fnhum.2012.00200/full
Matlab Bayes Factor Toolbox	Bart Krekelberg via GitHub	https://github.com/klabhub/bayesFactor
UnivarScatter plot function	Manuel Lera Ramirez via GitHub	https://github.com/manulera/UnivarScatter

RESOURCE AVAILABILITY

Lead contact

Further information and requests for resources should be directed to the lead contact, PD Dr. Dr. Björn H. Schott (bschott@lin-magdeburg.de; bjoern-hendrik.schott@dzne.de).

Materials availability

This study did not generate plasmids, mouse lines, or unique reagents.

Data and code availability

- **Code:** The code generated in the course of data analysis is available from the lead contact's GitHub site (GitHub: https://github.com/bhschott/DCM_MemoryEncoding).
- **Data:** DCM results reported in the present study and the corresponding group-level fMRI results (novelty and subsequent memory contrasts) are available from OSF (OSF: <https://osf.io/ktqy6/>). The single subjects' raw MRI data reported in this study cannot be deposited in a public repository due to restrictions imposed by the local ethics committee and EU data protection regulations. To request access, contact please contact the **lead contact** (bschott@lin-magdeburg.de; bjoern-hendrik.schott@dzne.de).
- Any additional information required to reanalyze the data reported in this paper is available from the **lead contact** upon request.

EXPERIMENTAL MODEL AND STUDY PARTICIPANT DETAILS

Participants

In the present study, we investigated three cohorts of participants, with the first cohort consisting of neurologically and psychiatrically healthy young adults (cohort 1: 117 young), and the other two cohorts including both young and older healthy participants (cohort 2: 58 young, 83

older; cohort 3: 64 young, 84 older). Participants were recruited via billboards, public outreach events of the Leibniz Institute for Neurobiology and local newspapers (for details on recruitment see^{30,57}). All participants were right-handed according to self-report and fluent in German. With the exception of two young participants in cohort 2 (one South Asian, one South American) and one young participant in cohort 3 (Middle Eastern), all participants were of European ancestry. The Mini-International Neuropsychiatric Interview (M.I.N.I.⁹⁸; German version by⁹⁹ was used to exclude present or past psychiatric disorders. Further contraindications for participation included alcohol or drug abuse or the use of neurological or psychiatric medication. Data from sub-cohorts of the current study population have been reported in previous studies (cohort 1:¹⁰⁰; cohort 2 and 3:^{30,57}). Importantly, the analyses performed here have not been conducted in the previous publications, and cohort 3 included 40 additional participants whose data have not been reported previously. Detailed demographic data are summarized in Table 1.

Informed consent and ethics approval

Written informed consent was obtained from all participants in accordance with the Declaration of Helsinki,¹⁰¹ and the study was approved by the Ethics Committee of the Otto von Guericke University Magdeburg, Faculty of Medicine (Approval number 33/15).

METHOD DETAILS

Experimental paradigm

During the fMRI experiment, participants performed an incidental visual memory encoding paradigm, using an indoor/outdoor judgment as encoding task.⁸ In cohort 1,^{100,102,103} the trial timings were slightly shorter compared to cohorts 2 and 3, where we employed the adapted version of the paradigm also used in the DELCODE study^{23,49,104} (see Table 1 for an overview of differences in trial timings and acquisition parameters). Subjects viewed photographs of indoor and outdoor scenes, which were either novel (44 indoor and outdoor scenes each) or were repetitions of two pre-familiarized "master" images (one indoor and one outdoor scene). Participants performed an "indoor" versus "outdoor" judgment on the images via button press. Each picture was presented for 2.5 s, followed by a variable delay ranging from 0.50 to 2.50 s in cohort 1 and from 0.70 s to 2.65 s in cohorts 2 and 3. The trial timing followed a near-exponential jitter and was optimized to improve estimation of the trial-specific BOLD responses.¹⁰⁵

Approximately 70 min (cohorts 2, 3) to 90 min (cohort 1) after the start of the fMRI session, participants underwent a computer-based recognition memory test outside the scanner, during which they were presented with photographs from the fMRI encoding phase (*old*; $n = 88$ plus the two master images), randomly intermixed with previously unseen (*new*) images ($n = 44$). Participants reported their memory confidence orally on a five-point rating scale from 1 ("definitely new") to 5 ("definitely old"), and the overt responses were recorded by an experimenter. For details, also see Assmann et al.¹⁰⁰ and Soch et al.^{23,30}

MRI data acquisition

Structural and functional MRI data were acquired on two Siemens 3T MR tomographs (cohort 1 and 2: Siemens Verio; cohort 3: Siemens Skyra; see Table 1), using previously reported protocols (cohort 1: see¹⁰⁰; cohorts 2 and 3: see²³ corresponding to the DELCODE MRI protocol, see^{49,106,107}

A T1-weighted MPRAGE image ($TR = 2.5$ s, $TE = 4.37$ ms, $\text{flip-}\alpha = 7^\circ$; 192 slices, 256×256 in-plane resolution, voxel size = $1 \times 1 \times 1$ mm) was acquired for co-registration and improved spatial normalization. In cohorts 2 and 3, phase and magnitude fieldmap images were acquired to improve correction for artifacts resulting from magnetic field inhomogeneities (*unwarping*, see below).

For functional MRI (fMRI), 206 T2*-weighted echo-planar images were acquired in interleaved-ascending slice order (see Table 1 for acquisition details). The complete study protocol also included additional structural MR images, which were not used in the analyses reported here (details available upon request).

fMRI data preprocessing

Data preprocessing and analysis was performed using Statistical Parametric Mapping (SPM12; University College London; <https://www.fil.ion.ucl.ac.uk/spm/software/spm12/>) running on MATLAB R2018b (Mathworks, Natick, MA). EPIs were corrected for acquisition time delay (*slice timing*), head motion (*realignment*) and magnetic field inhomogeneities (*unwarping*), using voxel-displacement maps (VDMs) derived from the fieldmaps (cohorts 2 and 3). The MPRAGE image was spatially co-registered to the mean realigned (cohort 1) or *unwarped* (cohorts 2 and 3) image and *segmented* into six tissue types, using the unified segmentation and normalization algorithm implemented in SPM12. The resulting forward deformation parameters were used to *normalize* EPIs into a standard stereotactic reference frame (Montreal Neurological Institute, MNI; voxel size = $3 \times 3 \times 3$ mm). Normalized images were spatially *smoothed* using an isotropic Gaussian kernel of 6 mm full width at half maximum (FWHM).

Additional behavioral measures of memory performance

The Verbal Learning and Memory Test (VLMT) and the Wechsler Memory Scale (WMS), subscale Logical Memory, were administered to the study participants as measures of explicit memory performance independent of the fMRI experiment (for details in cohort 1, see¹⁰²; for details in cohorts 2 and 3, see¹⁰⁸).

Verbal Learning and Memory Test (VLMT)

The Verbal Learning and Memory Test (VLMT) consists of two lists of 15 unrelated words, a study list and a distracter list.³⁷ The experiment included a learning phase and a recall phase. During the learning phase, participants were shown the words from the first list visually, one after another. When all words had been presented, participants were requested to write down every word they could remember. This procedure was repeated five times consecutively. Next, the distracter list was shown only once, followed by written recall. After presentation and recall of the distracter list, the recall phase began, where participants were asked to write down the words from the initial list. Additional recall phases took place after a 30-minute interval and after 24 hours.

Wechsler Memory Scale (WMS), Logical Memory

The Logical Memory subscale of the WMS (Wechsler Memory Scale) was implemented as an auditory version with slight modifications.³⁸ Participants were presented with two brief stories via headphones and were instructed to write them down immediately after listening. Recall tests were conducted 30 minutes and 24 hours later. The retrieved stories were evaluated for 25 items, representing details from the stories, by two independent experimenters. Thus, a maximum score of 25 points could be obtained for each story and recall time interval.

QUANTIFICATION AND STATISTICAL ANALYSIS

General linear model (GLM)-based fMRI data analysis

Statistical analysis of fMRI data was performed based on a two-stage mixed-effects model as implemented in SPM12. At the first stage (single-subject level), we used a parametric general linear model (GLM) of the subsequent memory effect that has previously been demonstrated to outperform the commonly employed categorical models.²³ The model included two onset regressors, one for novel images ("novelty regressor") and one for presentations of the two pre-familiarized images ("master regressor"). Both regressors consisted of short box-car stimulus functions (2.5 s), which were convolved with the canonical hemodynamic response function (HRF), as implemented in SPM12.

The regressor reflecting subsequent memory performance was obtained by parametrically modulating the novelty regressor with an arcsine function describing subsequent recognition confidence. Specifically, the parametric modulator (PM) was given by

$$PM = \arcsin\left(\frac{x - 3}{2}\right) \cdot \frac{2}{\pi}$$

where $x \in \{1, 2, 3, 4, 5\}$ is the subsequent memory report, such that $-1 \leq PM \leq +1$. By employing the arcsine transformation, *definitely* remembered (response "5") or forgotten (response "1") items were weighted more strongly than *probably* remembered (response "4") or forgotten (response "2") items (²³; Figure 2A). The model also included the six rigid-body movement parameters obtained from realignment as covariates of no interest and a constant representing the implicit baseline.

At the second stage of the model (across-subject level), contrasts of interest (novelty contrast: novel vs. master images; memory contrast: parametric memory regressor) were submitted to a one-sample t-test (cohort 1) and to ANCOVA models with age group as between-subjects factor and gender as a binary covariate of no interest (cohort 2, 3), respectively. The significance level was set to $p < 0.05$, whole-brain-corrected for family-wise error (FWE) at voxel-level, with a minimum cluster size of $k = 10$ adjacent voxels.

Dynamic causal modeling

Effective connectivity analysis was performed using DCM version 12.5 as implemented in SPM12. DCM uses an input-state-output model based on a bilinear state equation:

$$\dot{z} = \left(A + \sum_{j=1}^M u_j B^{(j)} \right) z + Cu$$

where \dot{z} is the temporal derivative of the state variable z , which describes neuronal activity resulting from intrinsic effective connectivity (A), changes in connectivity due to the contextual modulations (B) and the direct influence of the driving input u (C). The thus defined neuronal model is coupled to a biologically plausible neurovascular model of the BOLD response, and the coupled models are used to predict the BOLD time series in *a priori* defined volumes of interest (VOIs).

The goal of our DCM analysis was two-fold:

1. First, we aimed to assess the intrinsic effective connectivity of the PPA, the HC, and the Prc during novelty processing and the connectivity changes related to successful versus unsuccessful encoding of novel visual information.
2. Second, we aimed to assess, which connections within a temporo-parietal memory network are affected by age and whether age-related differences in effective connectivity are associated with memory performance in older adults.

Definition of regions of interest and time series extraction

ROIs were defined based on both anatomical and functional criteria, following previously described approaches^{32,33}. Anatomical constraints were defined using anatomical ROIs taken from Automated Anatomical Labeling (AAL), a canonical parcellation of the human brain,¹⁰⁹ as

implemented in the WFU PickAtlas (Wake Forest University; https://www.nitrc.org/projects/wfu_pickatlas/) or from previously described literature-based ROIs. Functional constraints were derived of memory and novelty contrasts in a previously published subset of cohorts 2 and 3 (106 young and 111 older participants;^{23,30}). Based on the meta-analytic evidence on encoding-related activations and deactivations⁴ and the age-related changes of those patterns,⁵ and guided by our own replication of those results, the ROIs were selected as follows: Previous DCM studies of memory encoding have also included prefrontal regions in their models. In the course of the present study, we also tested models that the mPFC, however, this did not improve the model fit. Please see also the [discussion](#) and [limitations](#) sections.

1. The PPA, which showed a pronounced response during both novelty detection and successful encoding³⁰ was used as the network's driving input region, given its well-replicated and relatively specific response to scene stimuli⁴⁶ and particularly to novel scenes.^{31,110} Given that the definition of the PPA is mainly based on its responsivity to scene stimuli rather than on anatomical landmarks, we restricted our ROI to a probabilistic definition of the PPA based on local maxima of activation clusters that were shown to respond to scene stimuli in previous studies (for details see⁹⁷). This probabilistic ROI was further restricted to the anatomical boundaries of the fusiform and parahippocampal gyri as defined by the AAL parcellation. Considering the intended use of the PPA as input region responding to all presentations of novel scenes (i.e., irrespective of subsequent encoding success), the thresholded SPM for the novelty contrast (novel > master images) was multiplied with the mask of the PPA, yielding a ROI for the PPA.
2. The HC has repeatedly been shown to respond more strongly to subsequently remembered compared to subsequently forgotten information in both young and older adults,^{4,5} a finding replicated in the present study ([Figure 2](#)). The ROI for the HC was thus defined by multiplying the thresholded SPM for the memory contrast (positive effects of the parametric memory regressor) with the anatomical boundaries of the HC from the AAL atlas and with a sphere seeded at the local group maximum of the contrast within the right anterior HC ($[x\ y\ z] = [21\ -10\ -19]$; $r = 15\text{ mm}$). The focus on the anterior HC was based on previous observations that encoding-related anterior hippocampal activations can be robustly observed in older adults⁵ and are at the same time sensitive to memory decline in aging.²¹ Furthermore, by restricting the ROI to the anterior HC, we aimed to avoid confounds from potential blurring of activity from the PPA into the posterior hippocampus.
3. The Prc emerged as the region most robustly activating more strongly (or, deactivating less strongly) during successful memory formation in older rather than young adults ([Figure 2](#)), in line with previous meta-analytic observations.⁵ We thus inclusively masked the thresholded SPM for the age group contrast (older > young) from the second-level memory GLM with the AAL Prc mask. To exclude activations in more lateral parietal cortex and posterior cingulate cortex, we further restricted the Prc ROI to a sphere centered at the local maximum of the age contrast ($[x\ y\ z] = [6\ -64\ 38]$; $r = 18\text{ mm}$). The larger radius compared to the hippocampal ROI was chosen based on the larger size of both the anatomical structure and the activation cluster.

To improve signal-to-noise ratio (SNR), we further restricted the ROIs to voxels with an uncorrected $p < 0.25$ on the respective contrast in the first-level GLM of each subject. The first eigenvariate time series were extracted from the thus obtained volumes of interest (VOIs) and adjusted for effects of interest (EOI) modeled and explained by the individual first-level GLMs.

As agreement of ROI locations across participants and cohorts has been deemed critical for DCM group analyses,¹¹¹ we aimed to ensure that our selection procedure yielded consistent results across cohorts and age groups. To this end, we computed the mean ROI coordinates for each subject and assessed their distribution within and across cohorts and age groups ([Table S8](#)).

First-level DCM analysis

The Parametric Empirical Bayes (PEB) framework implemented in SPM12^{25,26} allows for an efficient estimation of effective connectivity at group level by estimating the full model for each individual subject and pruning parameters that do not contribute to the model quality at the second level. In the present study, we employed bilinear DCM as implemented in the DCM PEB framework (²⁵; cf. Equation 2), similarly to previous descriptions of the approach.^{112,113}

The most general model which was estimated for each subject included the ROIs of the HC, PPA, and Prc, assuming full intrinsic connectivity, including self-connections. Novelty (i.e., presentation of novel, but not *master* images) was chosen as driving input to the PPA, and memory (the arcsine-transformed recognition memory responses representing encoding success) was included as a potential contextual modulator at all between-regions connections, but not at the self-connections ([Figure 1](#), right). The reason for not allowing for a modulation of self-connections was that the self-connections themselves turned out to be inconsistent across study cohorts ([Figure 4A](#)). Neural responses to the highly familiar *master* images were not included in the model and thus formed the implicit baseline.²⁵ The slice timing model implemented in the DCM PEB framework¹¹⁴ was set to the last acquired slice.^{25,115} This was motivated by the fact that the stimulus duration (2.5 s) was close to the TR, and mini-blocks of 2.5 s provided a better model fit than delta functions in first-level GLM analysis.²³ As a control, we also computed DCMs using $TR/2$ and TR/N_{slices} (i.e., number of slices) in the slice timing model. Explained variance of the first-level DCM analyses was substantially poorer for TR/N_{slices} (cohort 1: $p = 0.001$; cohort 2: $p = 0.057$; cohort 3: $p < 0.001$) and did not differ significantly for $TR/2$ (all > 0.161). Results of second-level PEB analysis for the model using $TR/2$ were qualitatively highly similar to the results of that using TR reported here.

Model estimation was performed using variational Laplace,¹¹⁶ which provides both, posterior estimates of connection strengths and the free energy approximation to the marginal likelihood.¹¹⁷ To yield a higher proportion of explained variance at the single-subject level, an iterative fit was performed, using the group mean parameter estimates as empirical priors (SPM function `spm_dcm_peb_fit.m`²⁶).

Group-level inference

Group-level inference on the effective connectivity within the temporo-parietal network was performed using Bayesian model reduction (BMR) and averaging (BMA), as implemented in the DCM PEB framework.^{26,116} After estimating each participant's full model (allowing for all potential connections and contextual modulations), the thus obtained DCMs were submitted to a second-level Bayesian GLM.^{26,118} To assess the strength of effective connectivity between the three ROIs as well as their modulation by successful memory performance and aging, the 15 parameters from model inversion (A-matrix and B-matrix) were submitted to BMR, followed by BMA. BMR compares the full model with a model space of nested models where one or more parameters (i.e., connections or contextual modulations) are switched off, keeping the parameters with the most evidence.^{26,116,119} Subsequently, BMA was employed to average the parameters across models, weighted by the evidence of each model.^{26,120} To test parameters across (or between) groups, we thresholded the posterior probability (PP) at 0.95 for any given parameter (or parameter difference) being larger than zero ($PP = \Pr(\theta > 0|y) > 0.95$). Parameters with supra-threshold PP in all three cohorts (or in cohorts 2 and 3, when testing for age group effects) were considered robust, and parameters with a PP > 0.95 in two cohorts were considered limited evidence. It must be noted that it is commonly recommended to use a threshold based on free energy, as this approach takes into account the posterior covariance during group model comparison.²⁶ However, this might on the downside potentially reduce generalizability due to subtle differences in parameter strength and thus differential pruning of parameters across cohorts. As testing for reproducibility of effects was a main goal of this study, we thus primarily reported marginal posterior probabilities and additionally computed the PPs based on the free energy thresholds for all parameters and age group differences to evaluate the agreement between marginal PPs and the (more stringent) free energy-based threshold.

Prediction of memory performance from DCM parameters

After group-level PEB analysis, we assessed whether the estimated parameters were associated with memory performance in older adults, and thereby contribute to assess the neurobiological underpinnings of cognitive aging.

Memory performance estimate

To obtain a measure of memory performance that takes into account recognition confidence, the area under the curve plotting hits (i.e., correctly recognized previously seen stimuli) against false alarms (i.e., falsely recognized previously unseen stimuli) was calculated as described previously.³⁰ To this end, o_1, \dots, o_5 and n_1, \dots, n_5 were defined as the numbers of old stimuli and new stimuli, respectively, rated as 1 ("definitely new") to 5 ("definitely old") in the delayed recognition test. Hit rates (H) and false alarm (FA) rates as functions of a threshold $t \in \{0, 1, \dots, 5\}$ are defined as proportions of old and new stimuli, respectively, rated higher than t :

$$H(t) = \frac{1}{O} \sum_{i=t+1}^5 o_i$$

$$FA(t) = \frac{1}{N} \sum_{i=t+1}^5 n_i$$

where $O = o_1 + \dots + o_5$ and $N = n_1 + \dots + n_5$. Note that $H(0) = FA(0) = 1$ and $H(5) = FA(5) = 0$. The hit rate can then be expressed as a function of the FA rate:

$$y = f(x), \text{ such that } y = H(t) \text{ and } x = FA(t) \text{ for each } t = 0, 1, \dots, 5$$

The area under the ROC curve (AUC) is then obtained by computing the integral of this function from 0 to 1:

$$A' = \int_0^1 f(x) dx = \int_0^1 H(FA) dFA$$

The value of this integral is referred to as AUC or A' ("A-prime") and provides a measure for memory performance, similar to the corrected hit rate, but also accounting for recognition confidence. When responses are completely random, A' equals 0.5, reflecting pure guessing. When all old items are recognized and all new items are correctly rejected, A' equals 1, reflecting 100% performance. An advantage over the frequently employed d' measure¹²¹ is that A' has finite values even in cases of zero or perfect performance.

To compare memory performance between young and older adults in cohorts 2 and 3, we computed two-sample t-tests, assuming unequal variances (i.e., Welch's tests). Bayes factors were computed using the Matlab Bayes Factor Toolbox.¹²²

Brain-behavior correlations

Given the high interindividual variability of the DCM parameters, which was suggestive for outliers (Figure 3), we computed outlier-robust Shepherd's P_i correlations³⁵ between connections that showed a robust age-group-related difference – as defined in 2.6.3 – and A' as a memory measure. Shepherd's P_i correlations have been proposed as a method to improve reliability of brain-behavior correlations, which have been criticized for their lack of robustness¹²³ and susceptibility to outliers.^{35,124} The approach is based on Spearman's correlation and includes a bootstrap-based estimation of the Mahalanobis distance, thereby allowing for an unbiased detection and exclusion of outliers. To comply

with the Bayesian framework of our DCM analyses, Wetzels' Bayes factors³⁶ were computed for all correlation coefficients, as implemented in the BayesFactor Toolbox for MATLAB¹²² (GitHub: <https://github.com/klabhub/bayesFactor>). As the sample size is reduced by the outlier exclusion of the Shepherd's *Pi* correlation, all Bayes factors were computed based on the effective sample size (i.e., not counting outliers). First, a likelihood function L was defined as described previously (see Wetzels & Wagenmakers,³⁶; Equation 13):

$$L(r, n, g) = \exp\left(\frac{(n-2)}{2}\log(1+g) - \frac{(n-1)}{2}\log(1+(1-r^2)g) - \frac{3}{2}\log(g) - \frac{n}{2g}\right)$$

where n is the sample size, r is the correlation coefficient, and g represents Zellner's g prior.^{125,126}

The Bayes factor BF_{10} , quantifying the relative likelihood of the alternative hypothesis over the null hypothesis, was computed by integrating the likelihood function over g and multiplying with a sample-size-dependent scaling factor:

$$BF_{10} = \frac{\sqrt{n/2}}{\Gamma(1/2)} \int_0^\infty L(r, n, g) dg$$

where $\Gamma(x)$ is the gamma function.

To further explore which DCM parameters were associated with memory performance in older and also young adults, we computed Bayesian Shepherd's *Pi* correlations between all DCM parameters and A' as the memory measure of interest as well as the performance measures from two independent memory tests (VLMT, WMS; see 7.4.4 for details).

We then estimated the overall evidence for the correlations across the study cohorts by averaging the correlation coefficients weighted by their effective sample sizes across cohorts, separately for young and older adults. To this end, correlation coefficients were first submitted to Fisher's z transformation to make them approximately normally distributed. Next, we computed the weighted mean z values

$$z_{\text{mean}} = \frac{1}{N} \sum_{j=1}^k z_j \cdot n_j$$

where z_{mean} is the weighted mean z -transformed correlation coefficient, N is the total effective sample size across all cohorts, k is the number of cohorts, z_j is the j^{th} z -transformed correlation coefficient, and n_j is the j^{th} effective sample size (i.e., the sample size after outlier exclusion by the Shepherd's *Pi* correlation). Weighted mean z -values were then transformed to the corresponding correlation coefficients using the inverse Fisher's z -transformation. Next, we computed the combined Bayes factors from all samples as described above, using N (i.e., the total effective sample size over all cohorts) as sample size (for a similar approach with t -test statistics, see Nikolakopoulos & Ntzoufras⁸³). The resulting weighted mean correlation coefficients and cumulative Bayes factors are reported in Tables S9 and S10.